

Imaging of Cardiovascular Elasticity



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Imaging of Tissue Elasticity
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Cardiovascular Deformation Imaging. *part 1: vascular*

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7. Conclusion



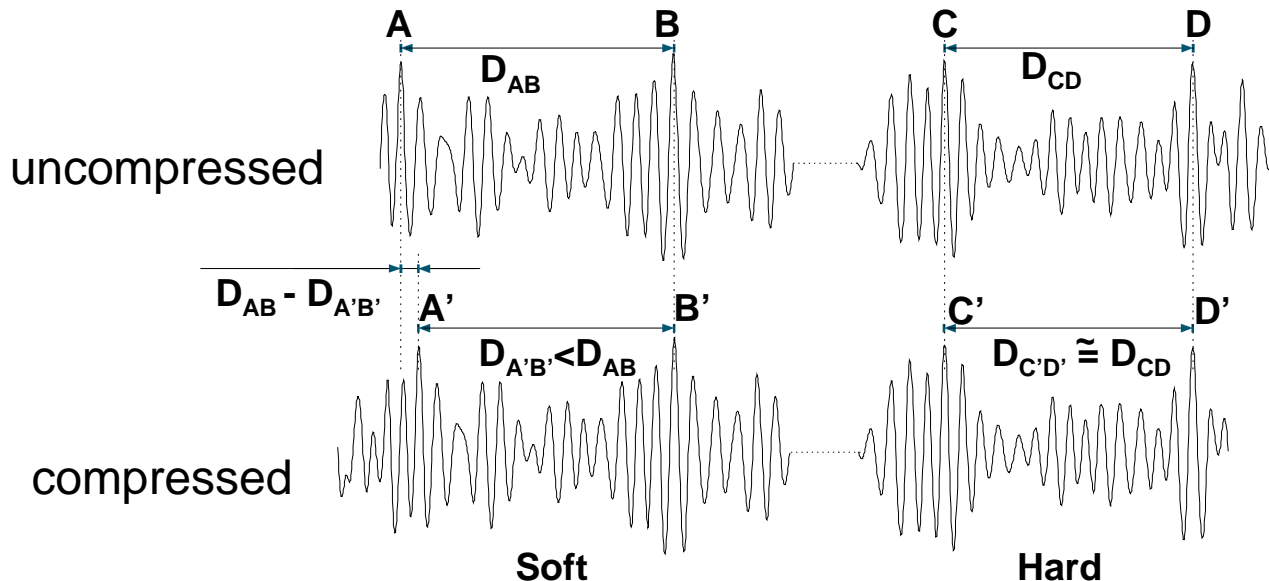
1. Elasticity Imaging

- Elastography: assessment of strain of tissue as a result of a controlled deformation. The response of the tissue is function of its mechanical properties.
- Strain Imaging: assessment of strain of tissue as a result of a physiologic deformation (blood pressure, muscle contraction). The strain is related to the mechanical properties or the function of the tissue.
- Different methods to detect strain:
 1. rf or envelope based elastography.
 2. TDI based strain/strain-rate imaging.
 3. Sonoelasticity Imaging.



RF or Envelope based elastography.

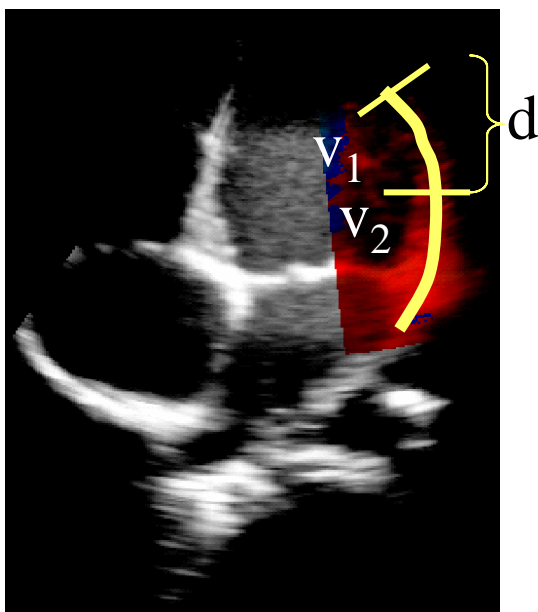
- Classical way of doing elastography as described in patent (1991).
- Cross-correlation analysis of windowed ultrasound signals.
- Finite difference to determine strain from time delays.





TDI based strain/strain-rate Imaging

- Method was first applied in cardiac imaging.
- Difference of tissue velocity in different regions along the ultrasound beam results in strain-rate.
- Strain-rate is converted to strain using integration.



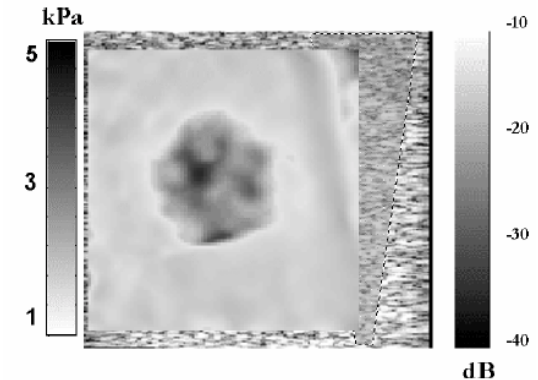
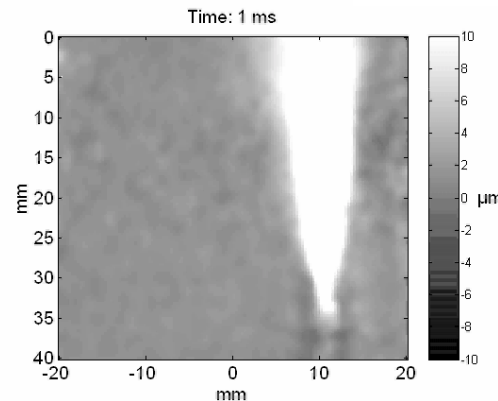
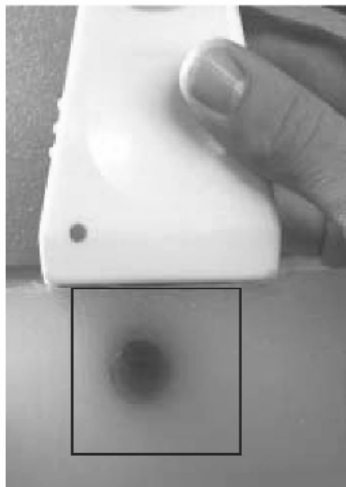
$$SR = (V2 - V1) / d$$



Sonoelasticity

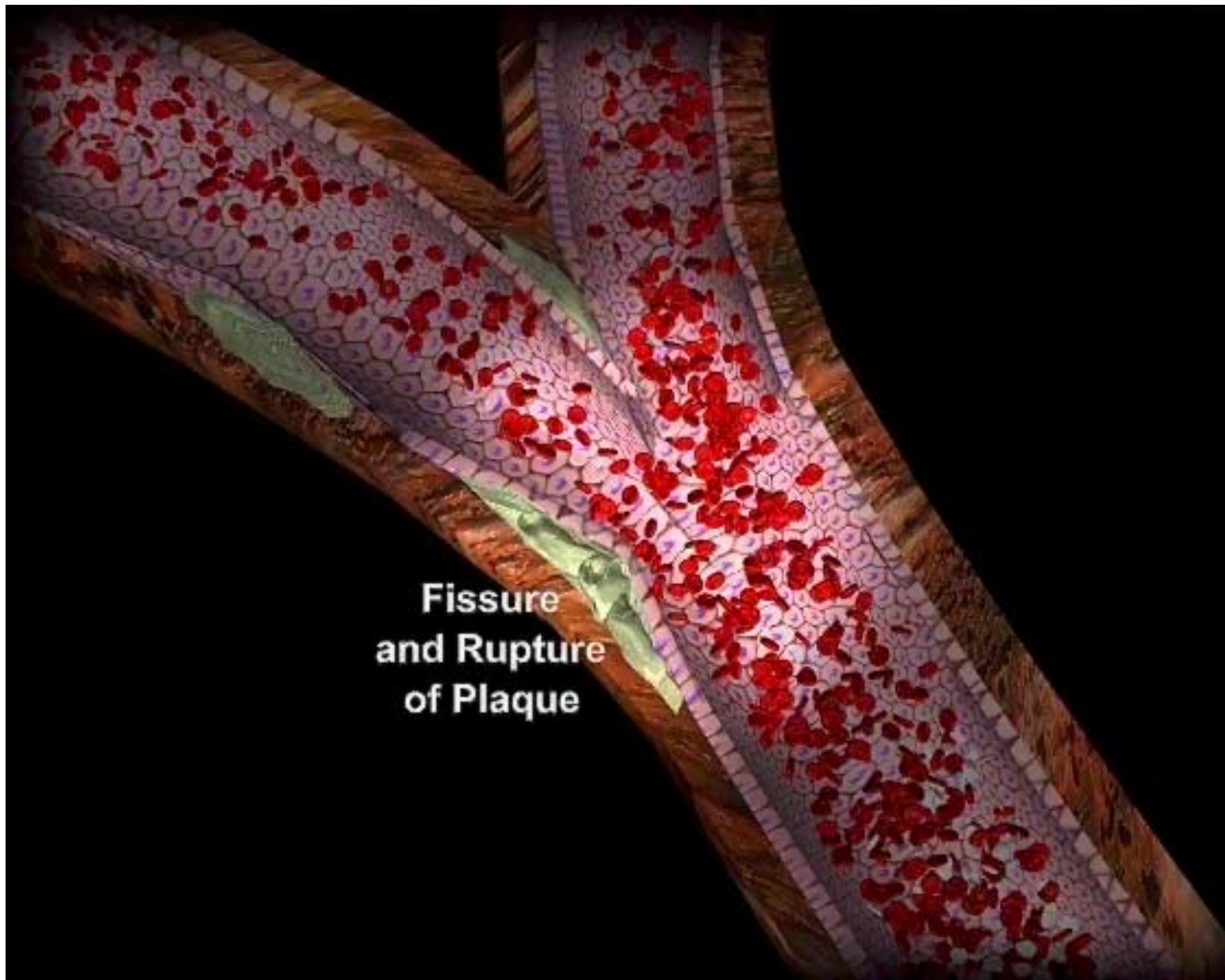
- A low frequency vibration is applied
- A small tissue inhomogeneity causes a disturbance in the shear wave.
- Supersonic Shear Imaging (SSI) is 'updated' version.

IEEE TRANSACTIONS ON ULTRASONICS, FERROELECTRICS, AND FREQUENCY CONTROL, VOL. 51, NO. 4, APRIL 2004



Bercoff et al, IEEE UFFC. 2004





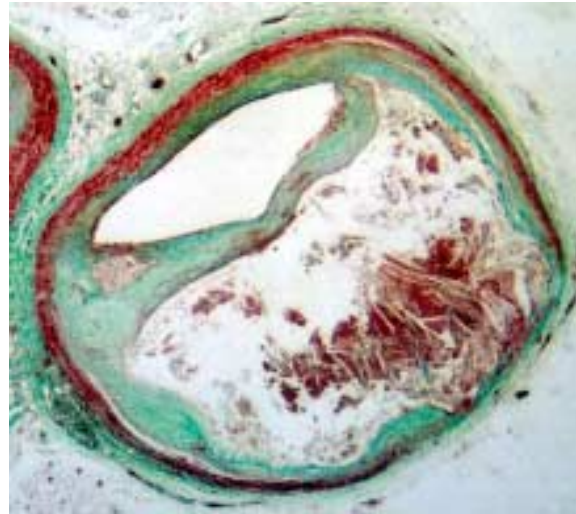
**Fissure
and Rupture
of Plaque**



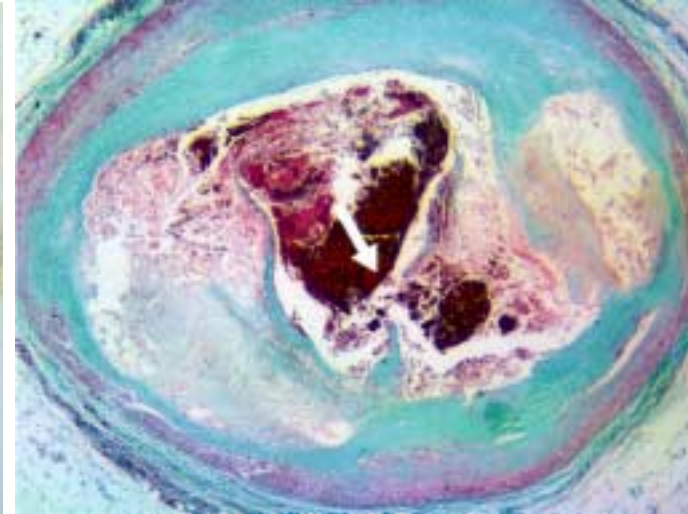
The way into the catastrophe



Small plaque



Big plaque

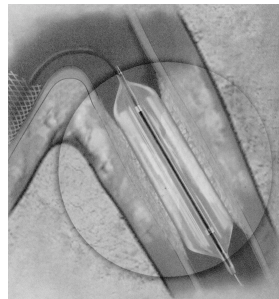


Infarction

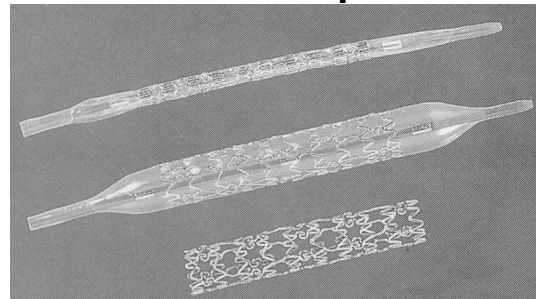


2. Mechanical properties of arteries

- Why do we need mechanical properties:
 1. Composition of the vessel wall and plaque
 2. Vulnerability of a plaque
 3. Effect of interventional procedures



PTCA



Stent

4. Effect of pharmaceutical treatment
 5. Age of thrombus
- What can we image in arteries and veins using elasticity imaging methods:



Composition

- The main components of atherosclerotic plaques have different mechanical properties (*Lee et al, Arteriosclerosis Thromb. 1992*)

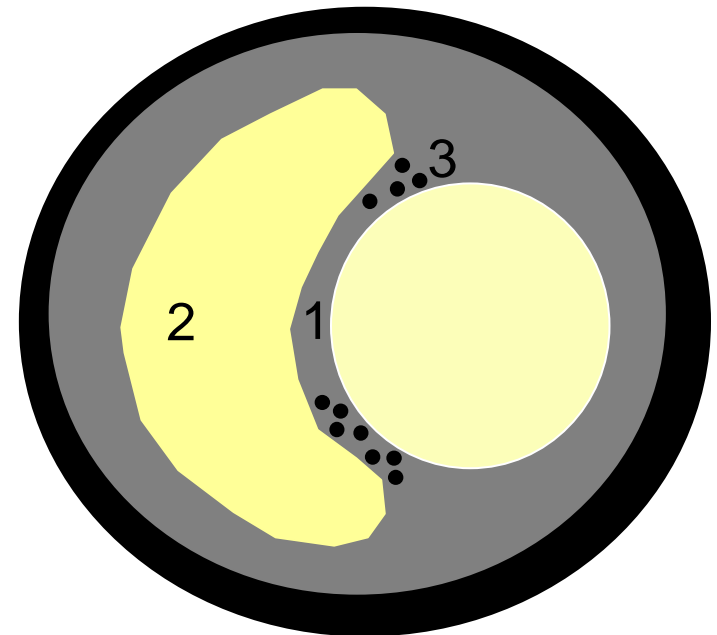
Tissue type	Modulus
non-fibrous	41 kPa
fibrous	82 kPa
calcified	355 kPa

- Caps with increased macrophage density are weaker than non-inflamed caps (*Lendon et al, atherosclerosis. 1991*)



Plaque vulnerability

- Plaque vulnerability is associated with:
 1. Thin fibrous cap
 2. Big lipid pool
 3. Inflammation (macrophage infiltration)
 4. High stress regions





Age of thrombus

- The age of a thrombus is the parameter that determines the strategy to dissolve it.

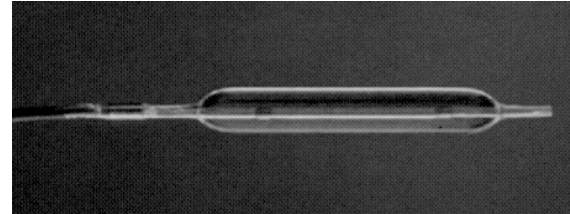
Pharmaceutical treatment

- Several therapies (like statin treatment) stabilize the plaque and does not affect the size of it.
- Interventional strategies are mechanical in nature and will affect the mechanical properties of the vessel wall and plaque.

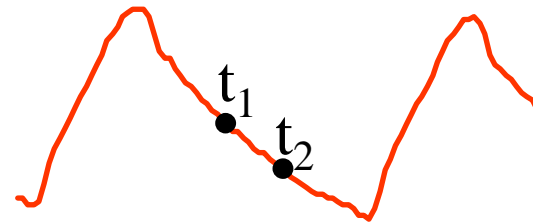


3. Sources for deformation in vascular applications

- Balloon



- Intraluminal pressure



- Deformation from outside





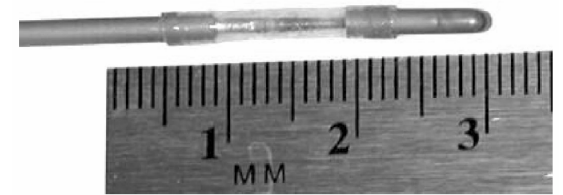
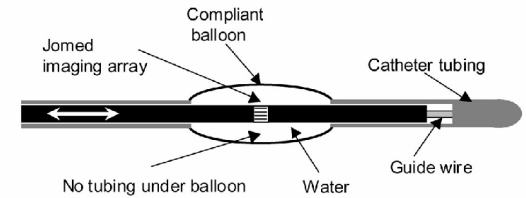
Balloon

- Two types of balloon are used:

1. Compliant balloon

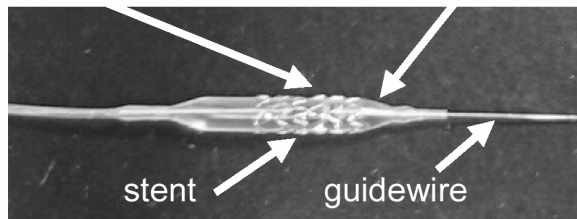
- Optimal relation between pressure and applied stress.
- Minimum cause of damage.

CHOI *et al.*: COMPLIANT BALLOON ULTRASOUND CATHETER



Choi et al, IEEE UFFC. 2002

Joined IVUS imaging array semi-compliant balloon



Choi et al, Proc IEEE Ultras Symp. 2002

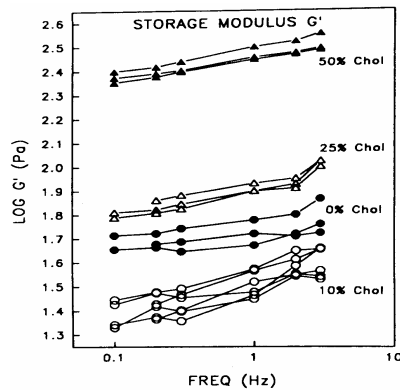
2. Non-compliant balloon

- Stress in tissue is unknown due to 'shielding' of the balloon.
- Used for monitoring interventional procedures

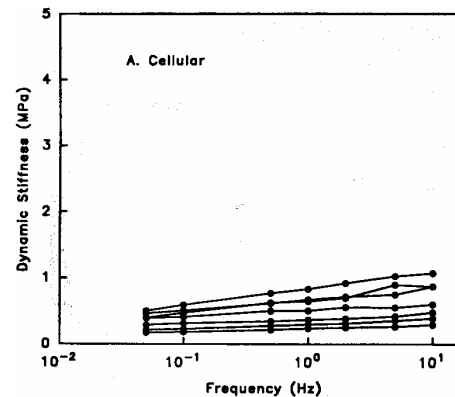


Intraluminal pressure

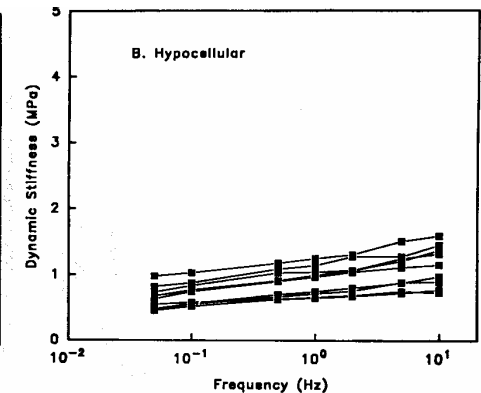
- Minimal invasive since it is already present.
- Excellent relation between pressure and applied stress.
- Dynamic (or semi-dynamic) instead of static excitation. However, ratio remains the same.
- Non-controllable.
- Acquisitions are disturbed by motion.



Loree et al,
Arteriosclerosis Thromb. 1994



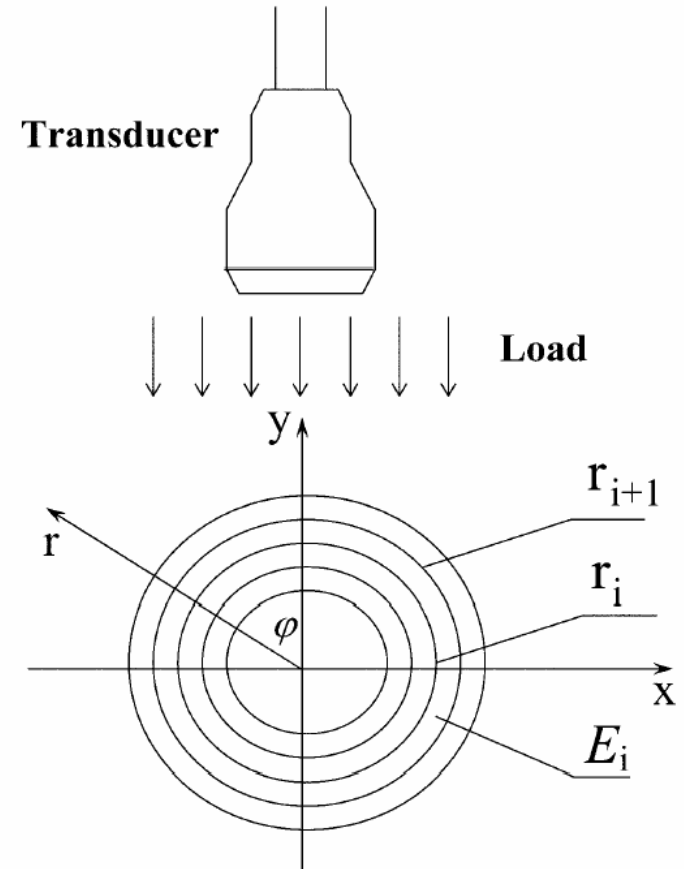
Lee et al, *Circulation.* 1991





Deformation from outside

- Only for superficial arteries
- Especially suited for clotted arteries (thrombosis).
- Correction needed for misalignment of ultrasound beam and radial strain vector.



Aglyamov et al, IEEE UFFC. 2004



4. Non-invasive vascular elasticity imaging

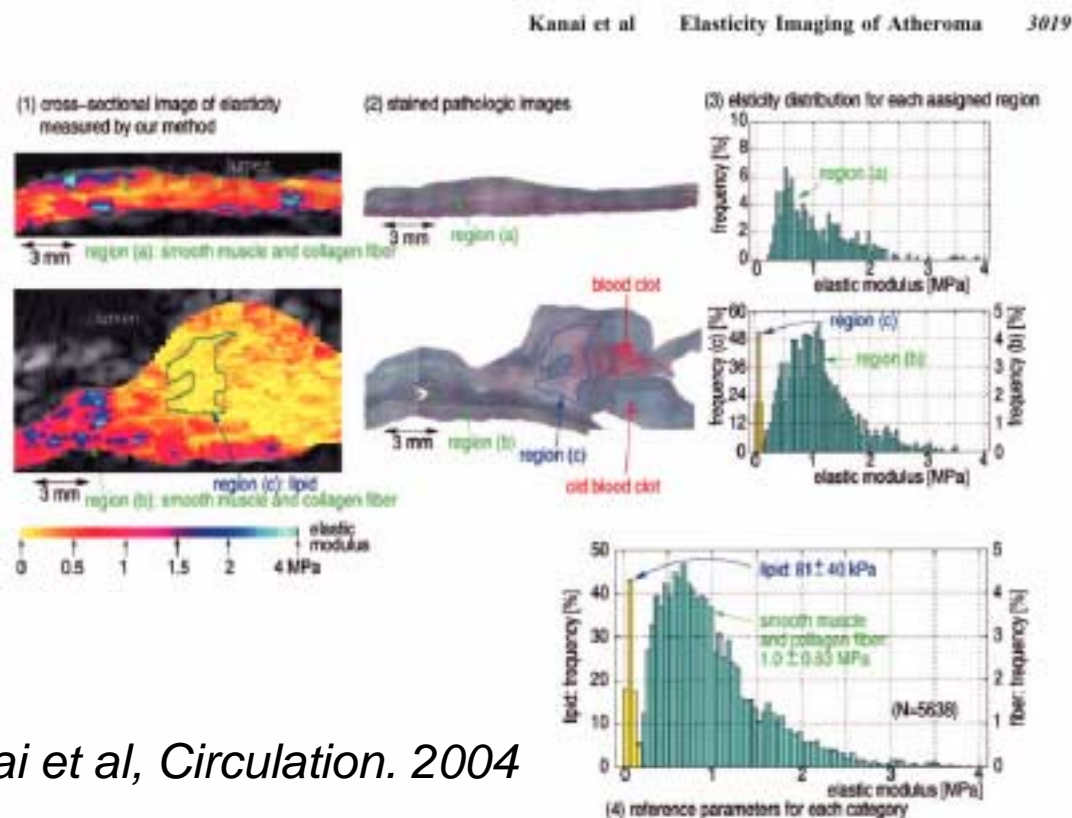
- Assessment of plaque composition in superficial arteries.
- Assessment of thrombus stiffness/age
- Arteries suitable for non-invasive approach:
 - Carotid artery
 - Femoral artery





Assessment of plaque composition I

- Parallel orientation of the transducer and artery: *in vitro* validation.

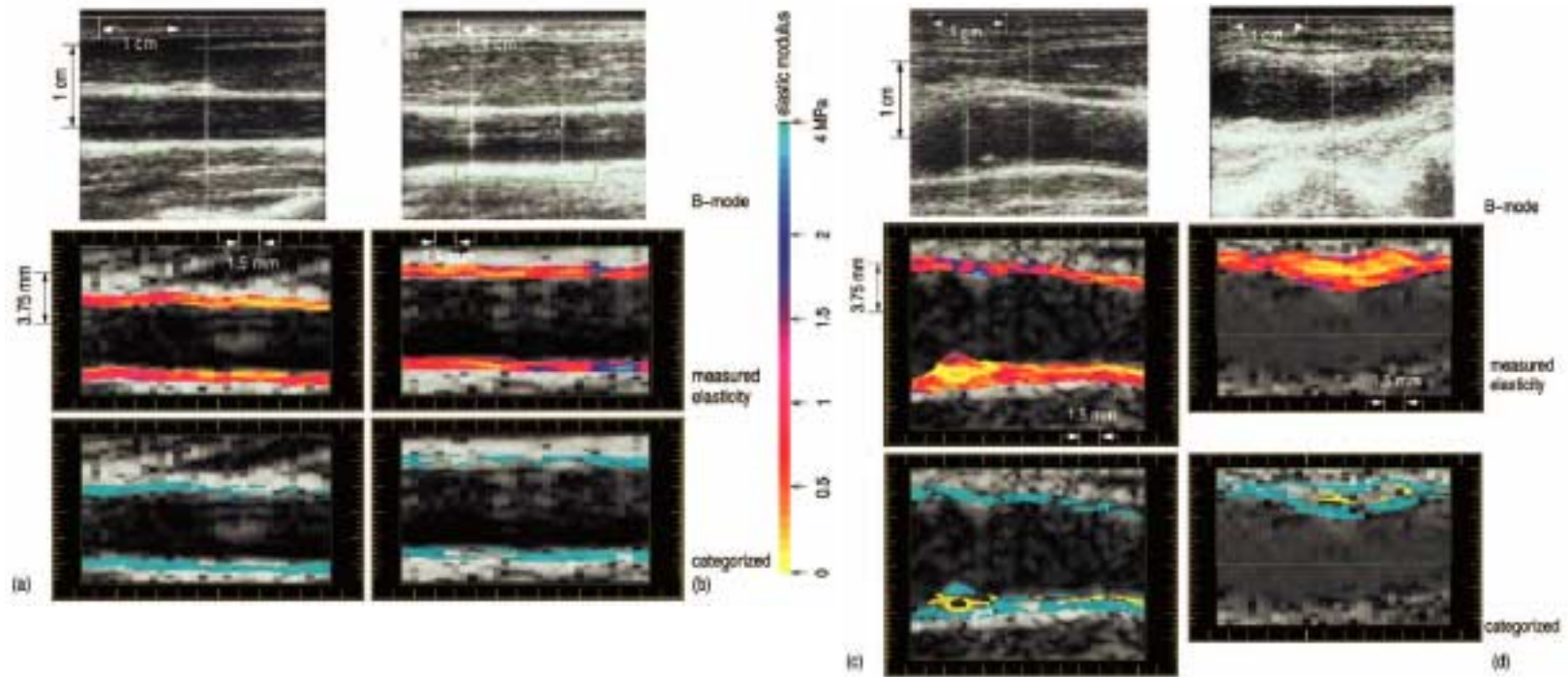


Kanai et al, *Circulation*. 2004



Assessment of plaque composition II

- Parallel orientation of the transducer and artery: *in vivo* application.

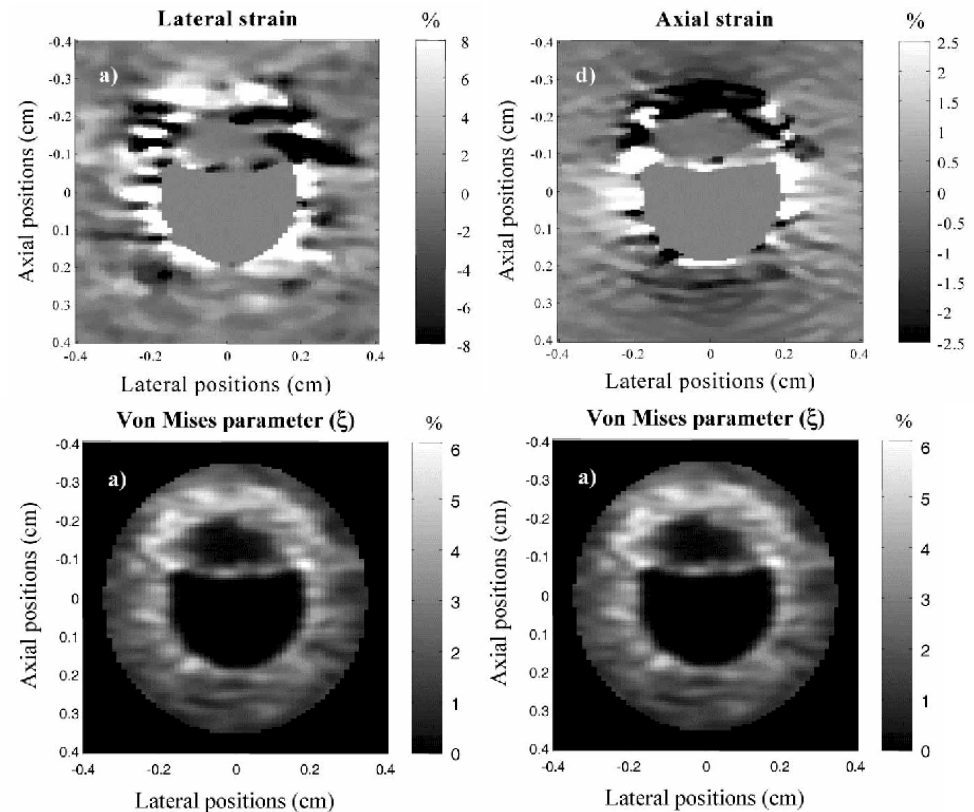


Kanai et al, Circulation. 2004



Assessment of plaque composition III

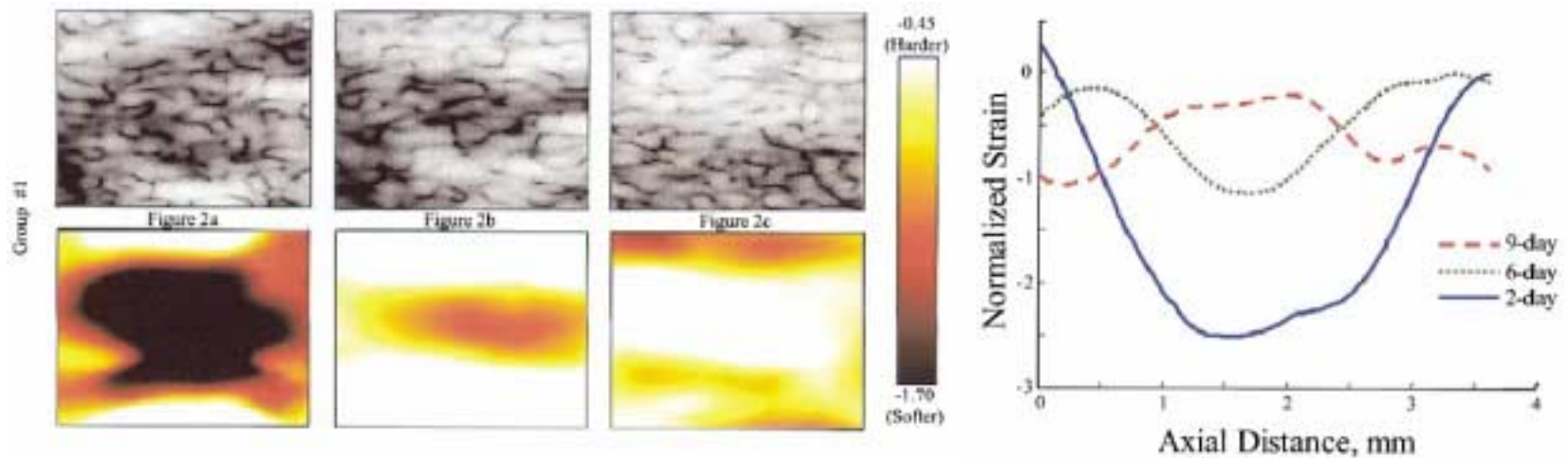
- Transducer orientation perpendicular to vessel axis *simulations.*



Maurice et al, IEEE Med Imag. 2004

Assessment of thrombus stiffness I

- Force is applied externally with the transducer.
- Evaluation of technique in vivo in rat model.

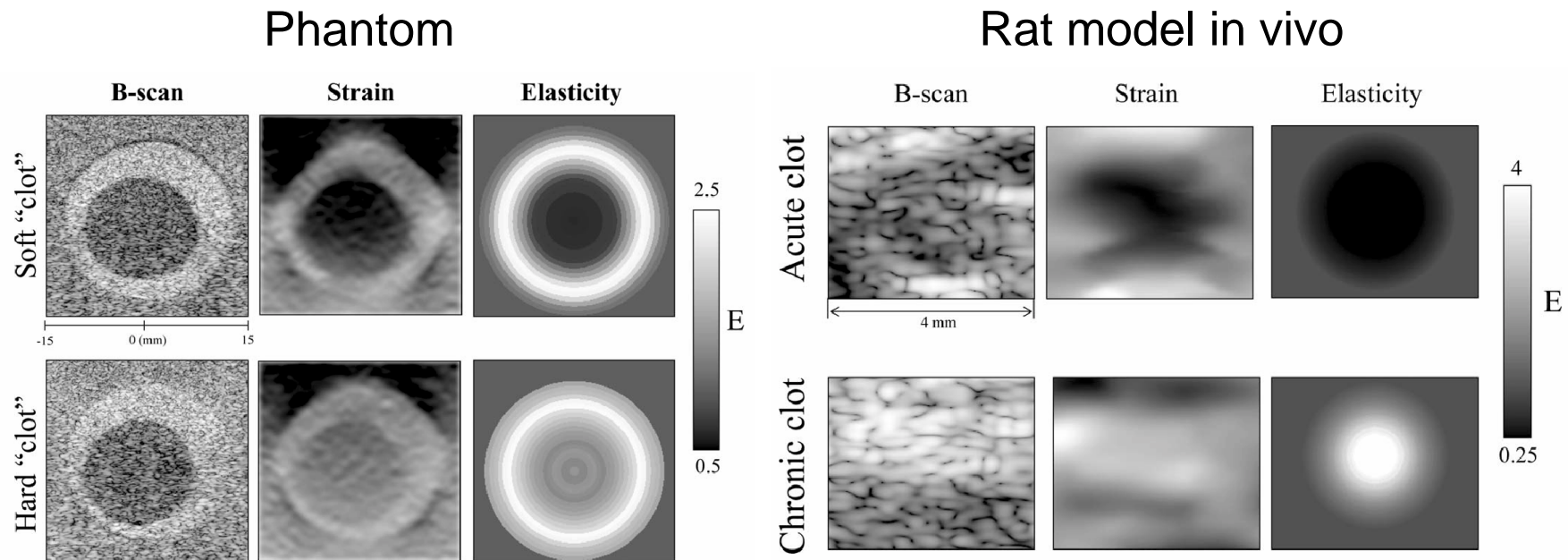


Emelianov et al, Ultras Med Biol. 2002



Assessment of thrombus stiffness II

- Layered cylinder model is used to estimate E .



Aglyamov et al, IEEE UFFC. 2004



5. Invasive vascular elasticity Imaging

- Using an intravascular catheter.
- Pulsatile pressure or balloon is used as force.
- Assessment of strain in larger vessels (diam >2mm).
- Especially used in coronary arteries.



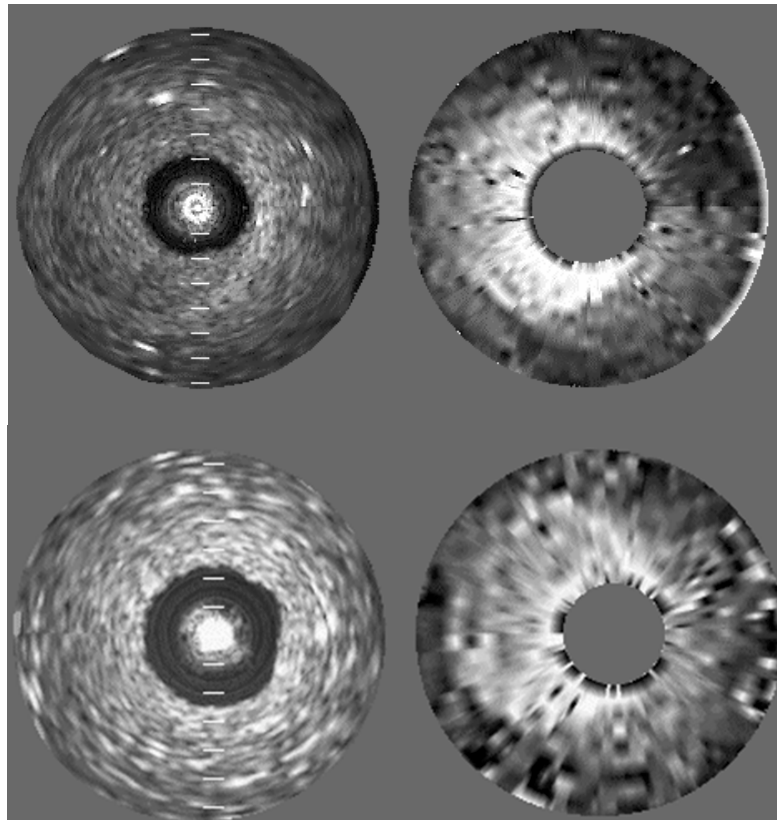
Validation in Phantoms

- Phantom studies:
 1. Flexible geometries and moduli
 2. Thick walled vessels to develop techniques
 3. Testing Influence of echogenicity
 4. Homogeneous phantoms allow theoretical studies (catheter position, SNR_E)
- Performed by various groups using different catheters and deformation sources



Validation in Phantoms

- Modified single element catheter using 'blood' pressure.

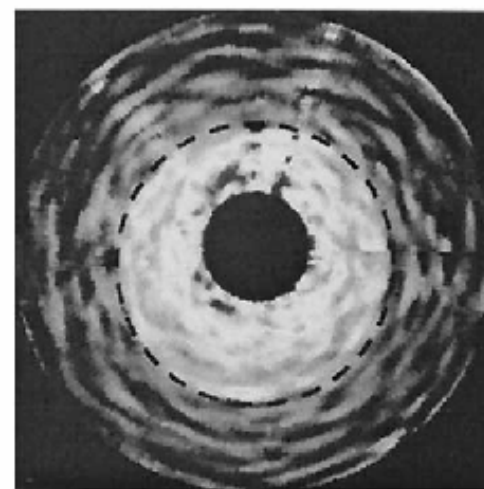
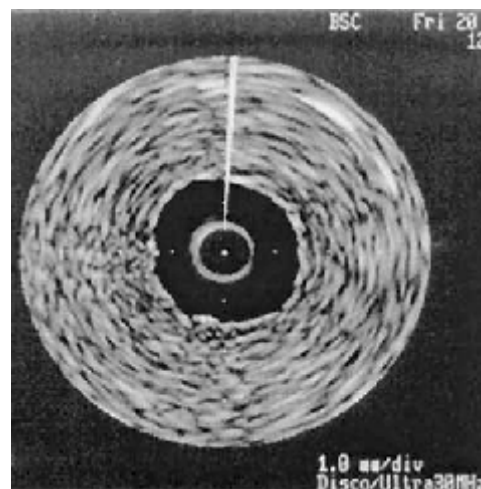
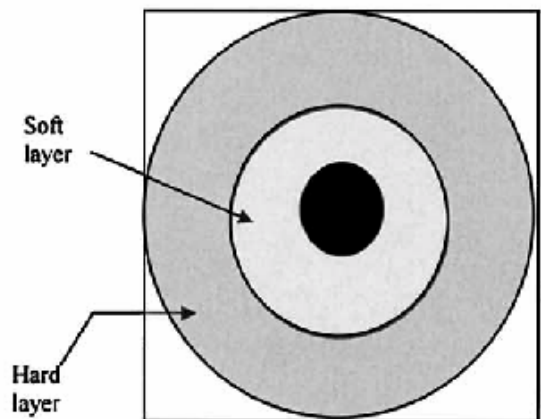


de Korte et al, Ultras Med Biol. 1997



Validation in Phantoms

- Single element catheter connected to commercial IVUS system
- Deformation due to increasing 'blood' pressure



Strain in %

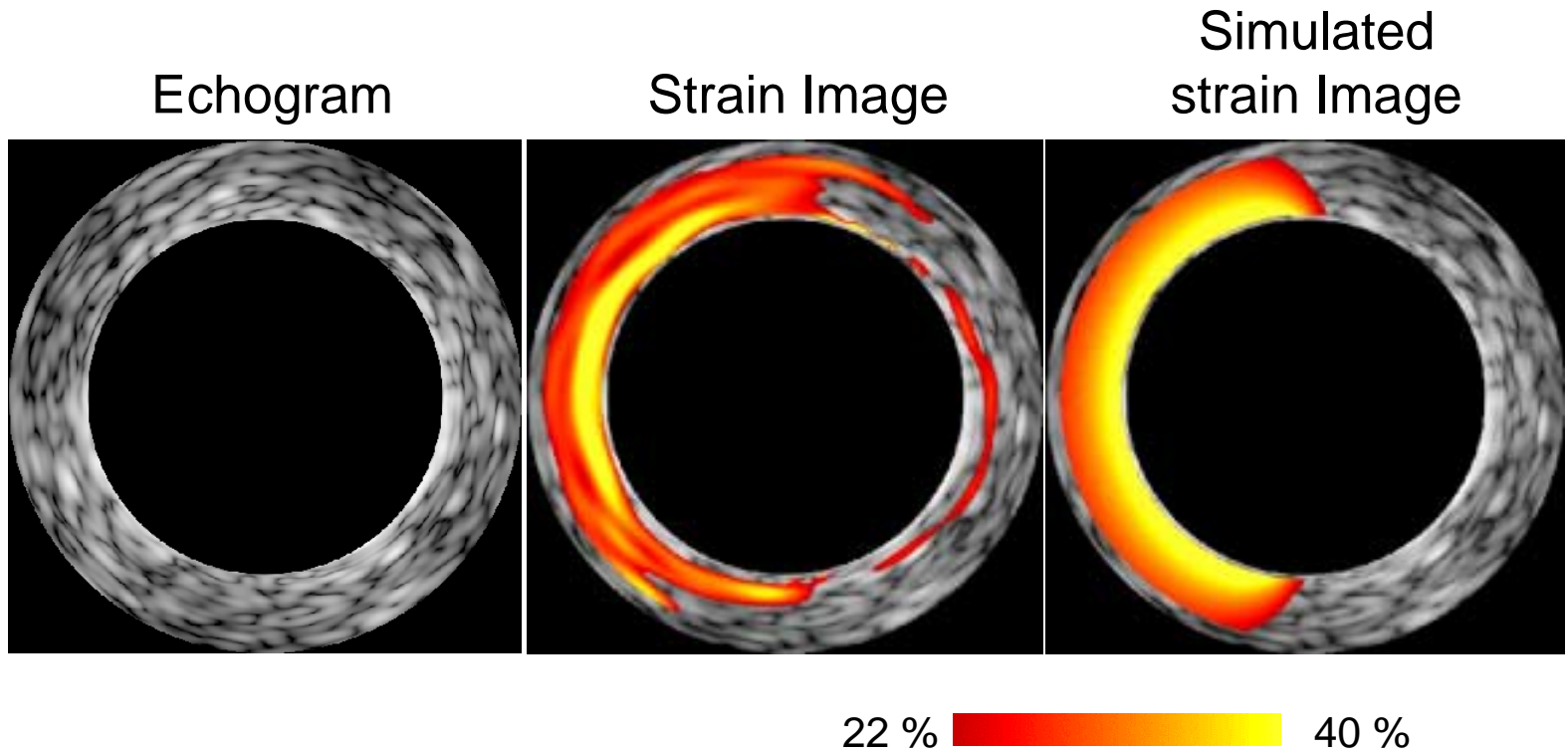


Brusseau et al, Ultras Med Biol. 2002



Validation in Phantoms

- Array catheter integrated with balloon



Courtesy M. O'Donnell et al, Ann Arbor, USA

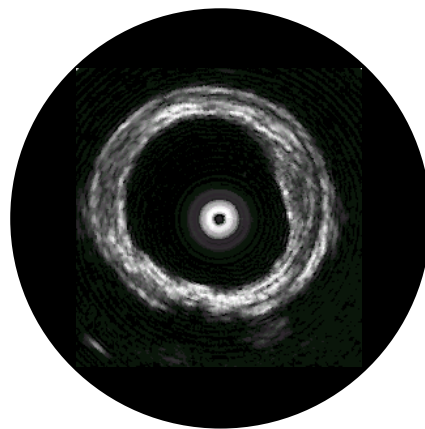


Ex-vivo validation

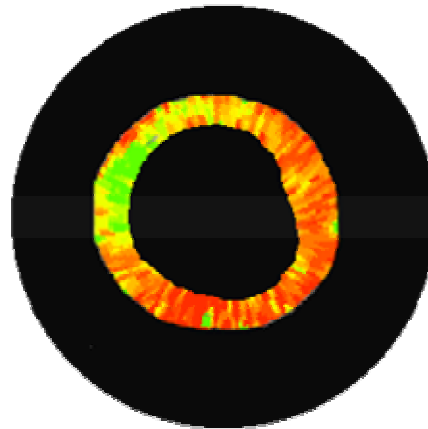
- Validation studies:
 1. Provides answer to question if technique works on real specimen
 2. Allows correlation with histology
 3. Provides tissue characterization properties
 4. Provides vulnerable plaque detection properties
- Performed by various groups using different catheters and deformation sources

Ex-vivo validation: feasibility I

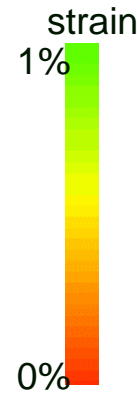
- Single element catheter and intraluminal pressure.
- Fibrous plaque in human femoral



IVUS



Elastogram



Hematoxylin
Eosin

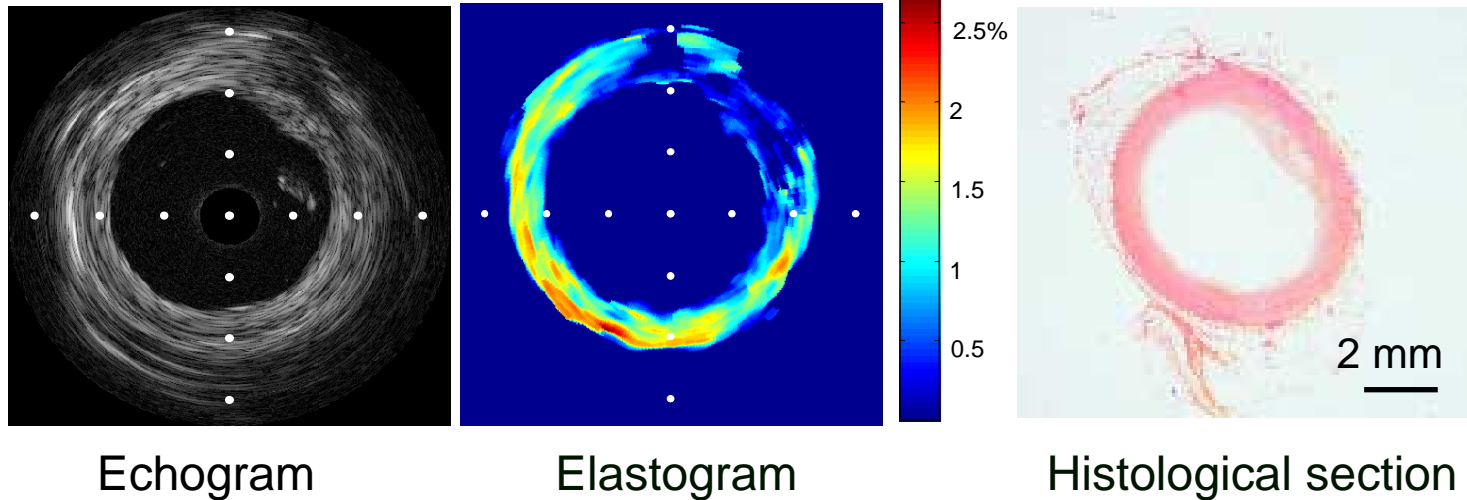
Elastic
van Gieson

de Korte et al, Ultras Med Biol. 1997



Ex-vivo validation: feasibility II

- Single element connected to commercial system.
- Fibrous plaque in carotid artery.

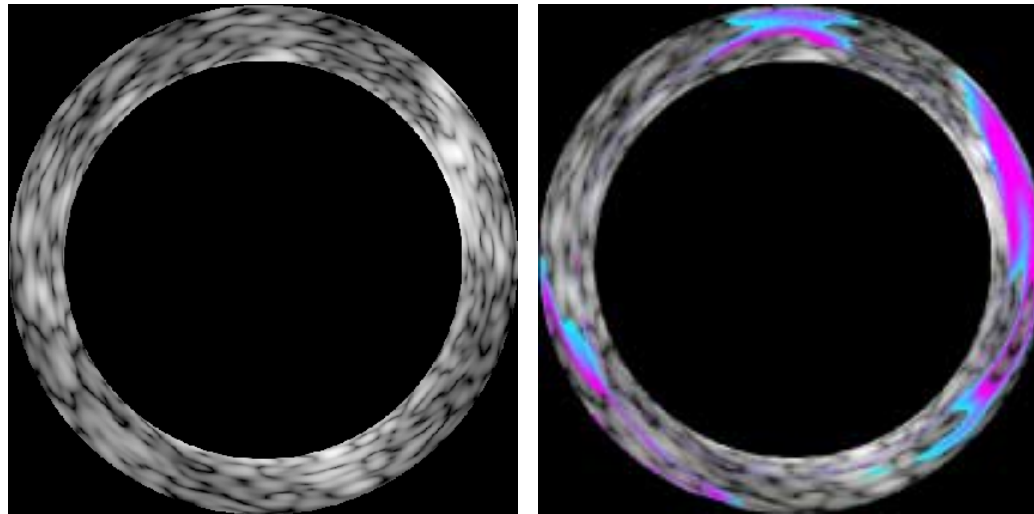


Brusseau et al, Ultras Med Biol. 2002



Ex-vivo validation: feasibility III

- Array catheter with integrated balloon.
- Fibrotic plaque in human femoral artery.
- Strain values higher than 21% are not shown



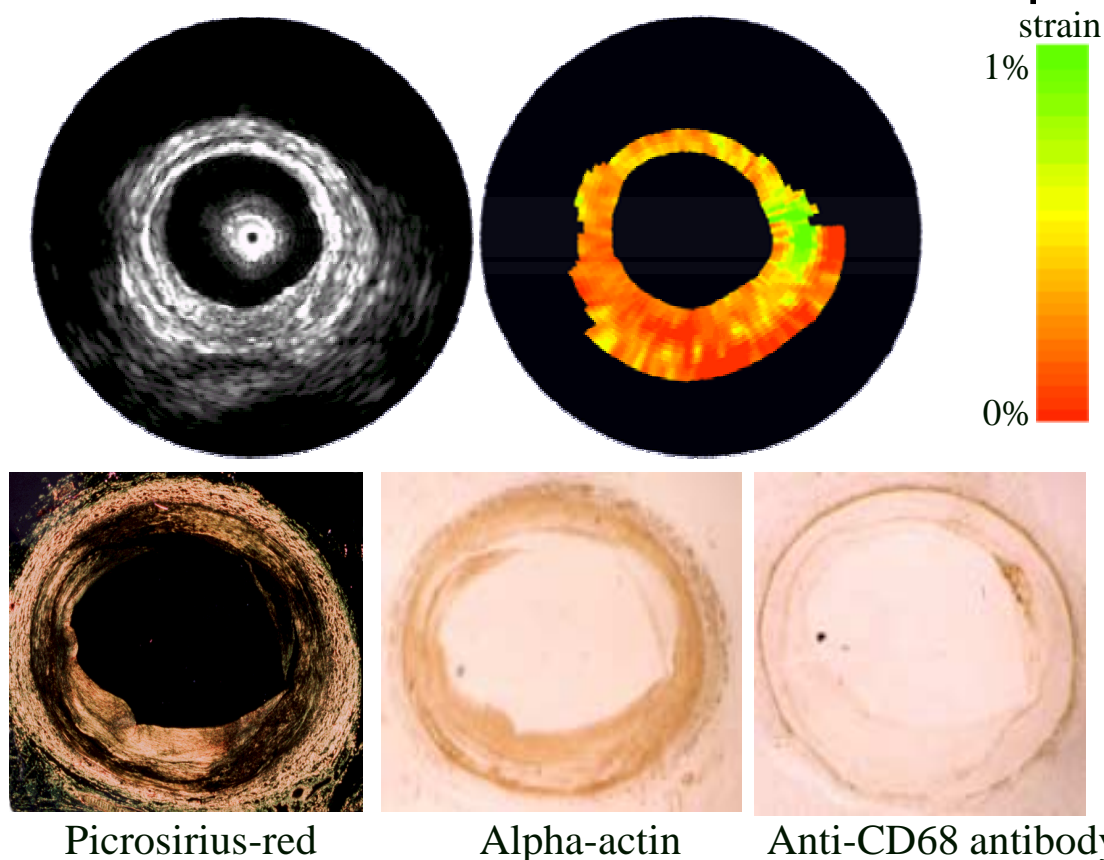
7 %  21 %

Courtesy M. O'Donnell et al, Ann Arbor, USA



Ex-vivo validation: validation I

- Single element catheter and intraluminal pressure

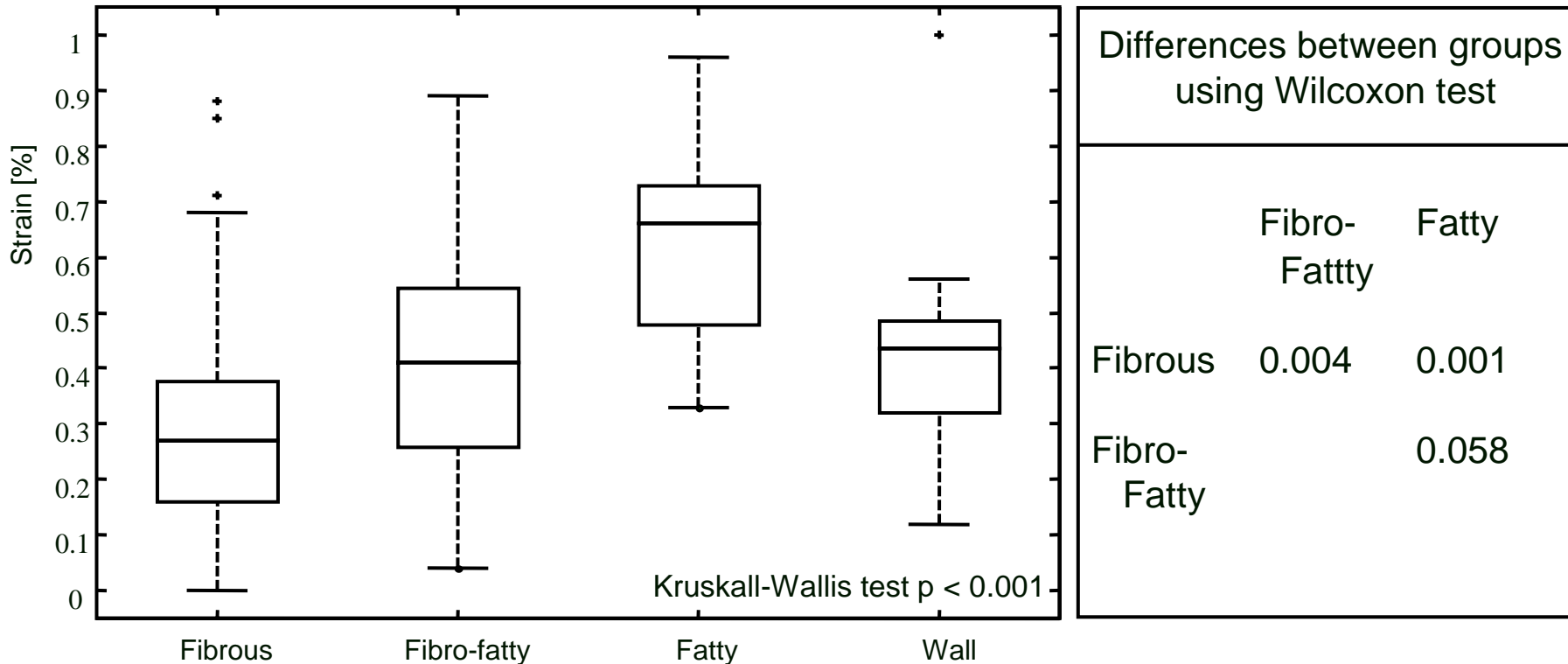


de Korte et al, Circulation. 2000



Ex-vivo validation: validation II

- Human femoral (n=9) and coronary (n=4) arteries with 125 regions segmented in 45 cross-sections

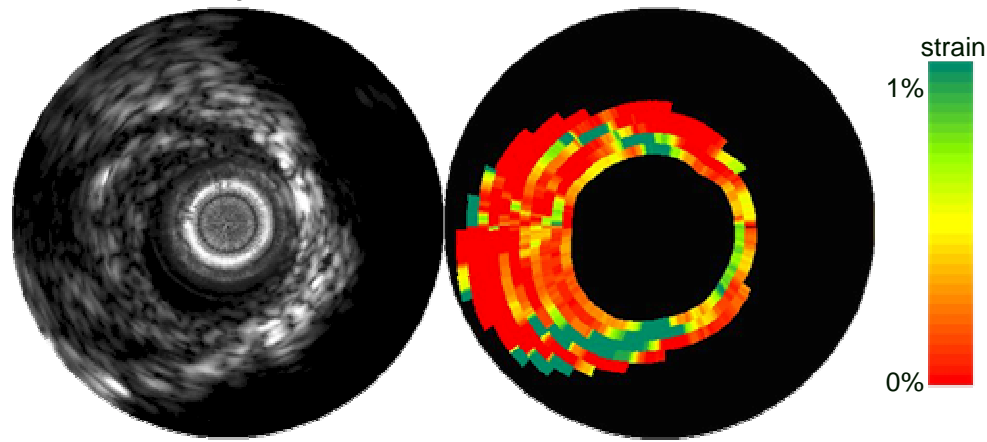


de Korte et al, Circulation. 2000



Ex-vivo validation: validation III

- Annular array catheter and intraluminal pressure



Picrosirius-red

Alpha-actin

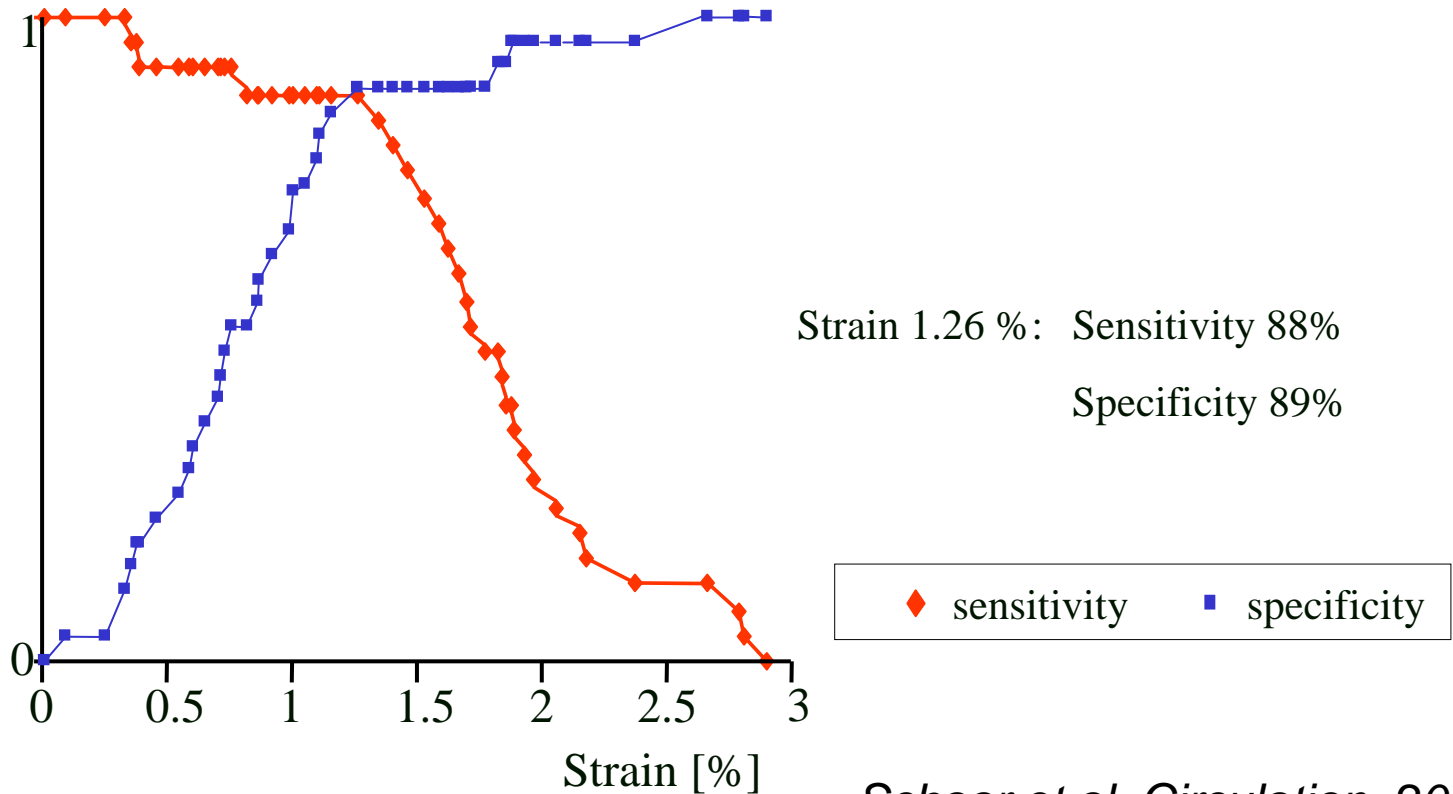
Anti-CD68 antibody

Schaar et al, Circulation. 2003



Ex-vivo validation: validation IV

- Sensitivity/specificity analysis to determine optimal threshold

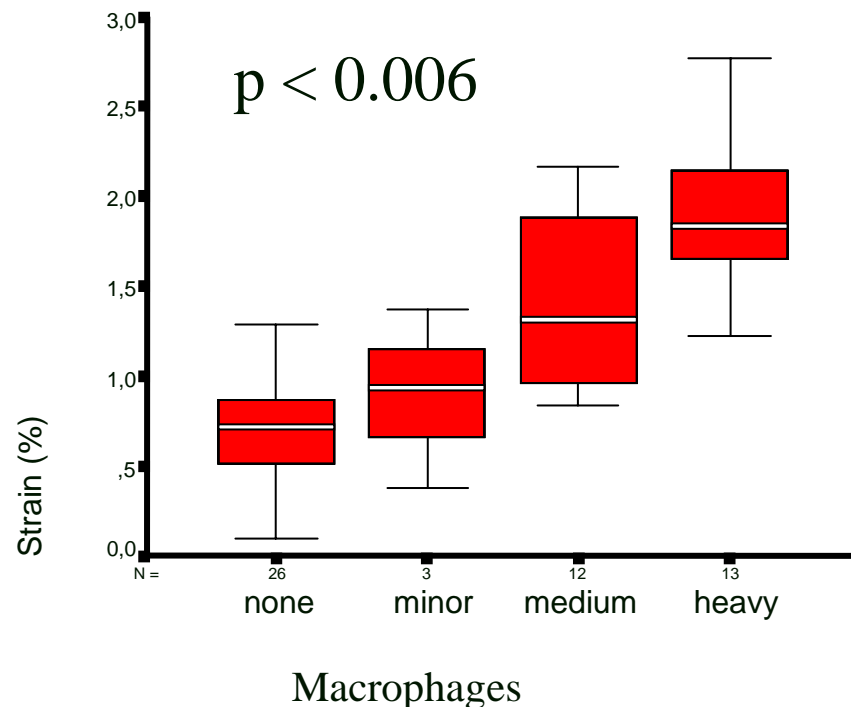
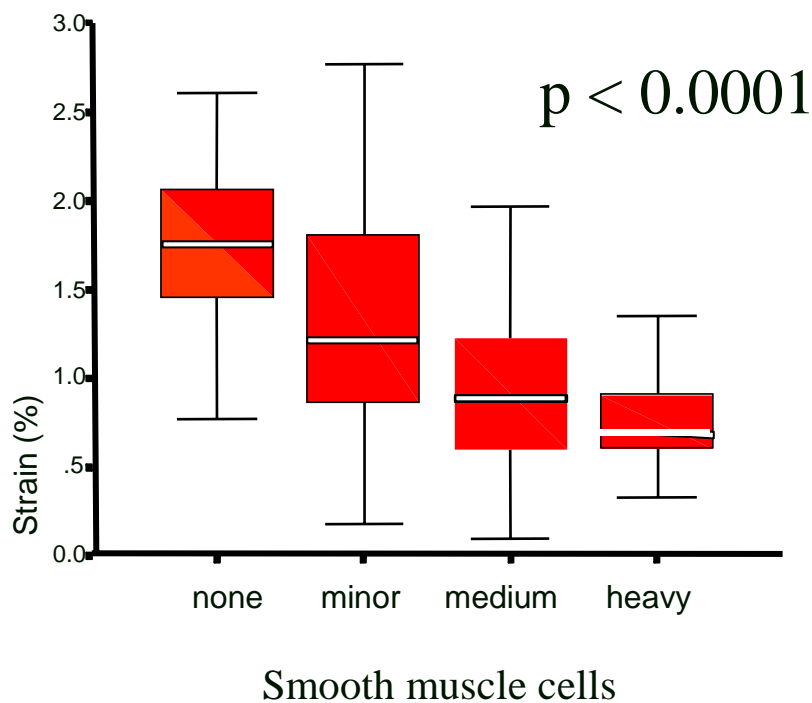


Schaar et al, Circulation. 2003



Ex-vivo validation: validation V

- Relation between strain value in high strain spot and plaque composition

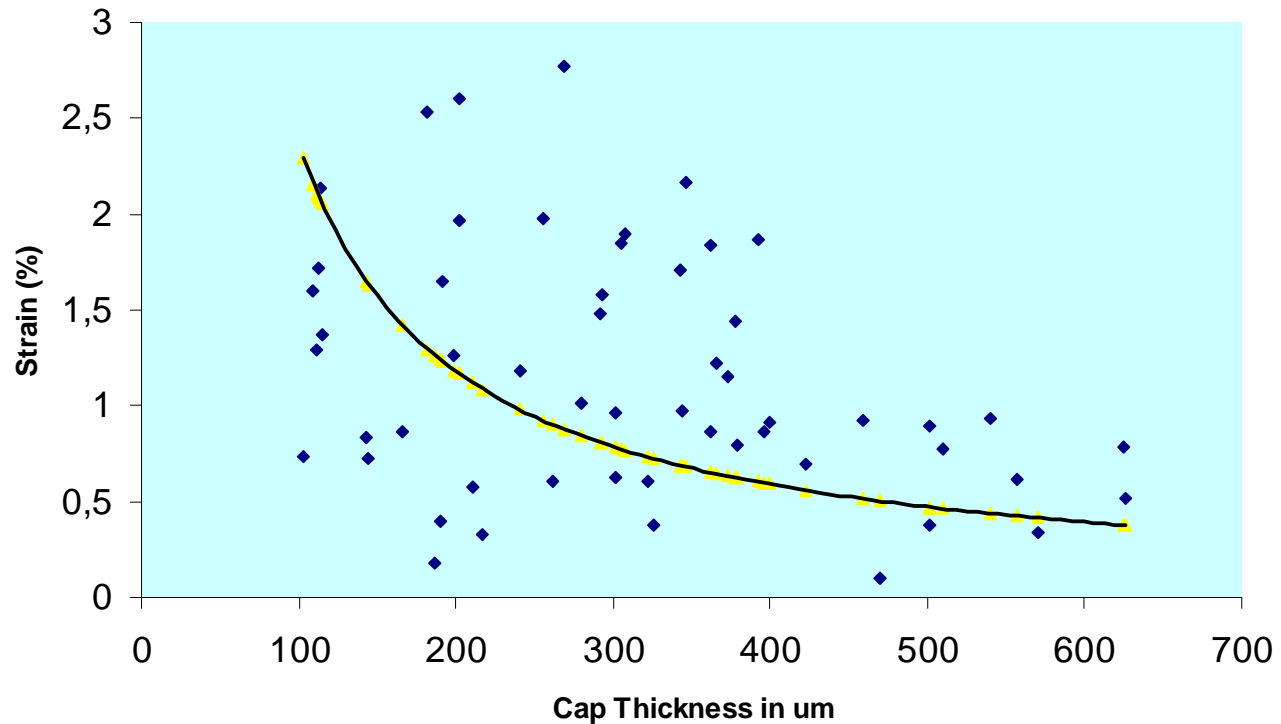


Schaar et al, Circulation. 2003



Ex-vivo validation

- Relation between strain value in high strain spot and cap thickness



Schaar et al, Circulation. 2003

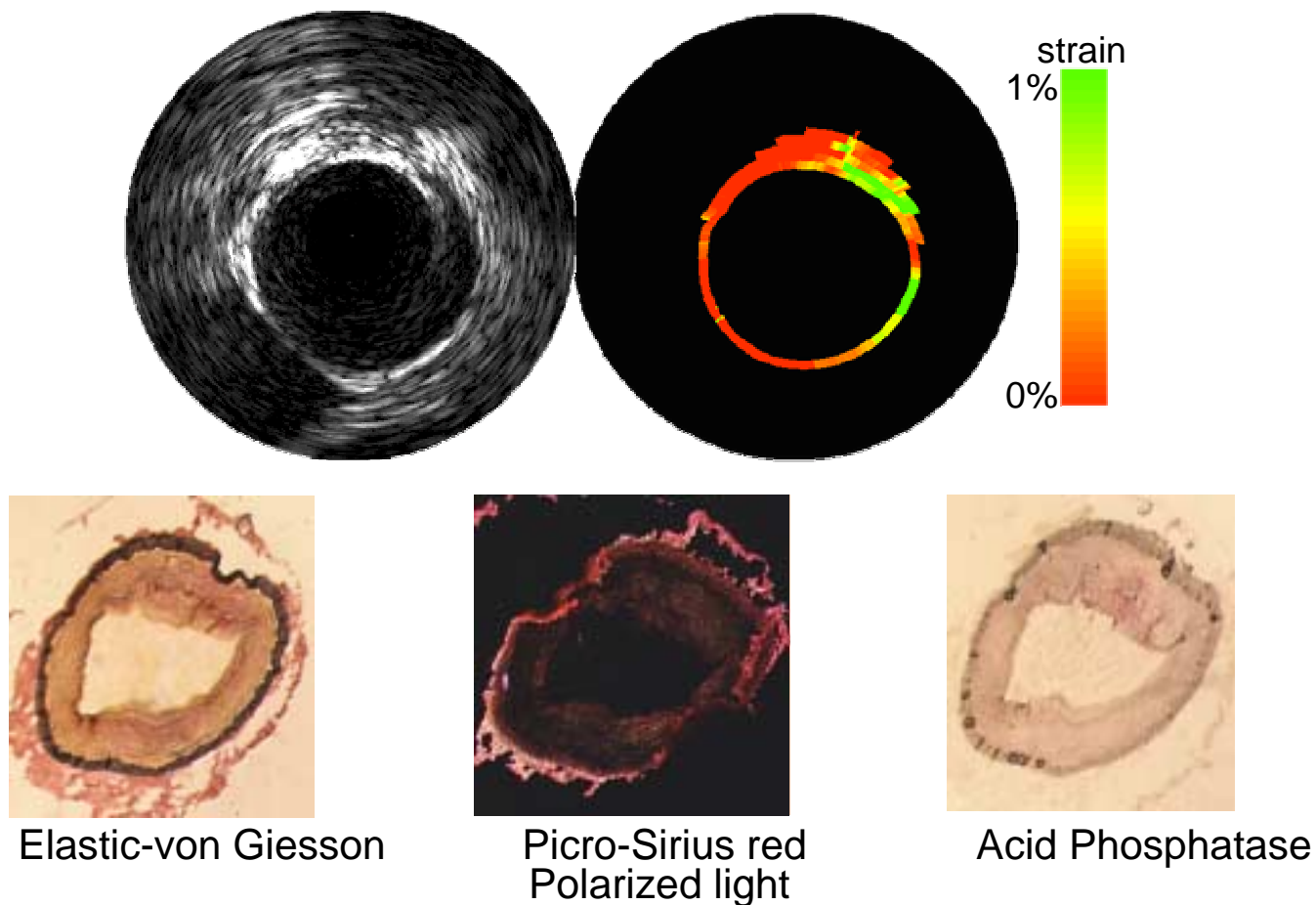


In vivo validation I

- Array catheter using intraluminal pressure as force.
- Yucatan Pig atherosclerotic model
- Acquisitions in femoral and iliac artery
- Histologic analysis for:
 1. Plaque composition
 2. Vulnerable plaque markers



In vivo validation II



de Korte et al, Circulation. 2002



In vivo validation III

- Relation between strain and plaque type

Mean strain value in total plaque area

Tissue	Strain [%]	
	mean	std
Normal segments (n=6)	0.21	0.09
Early fatty lesion (n=9)	0.46 [*]	0.17
Early fibrous lesion (n=3)	0.24	0.03
Advanced fibrous lesion (n=6)	0.22	0.04

* P=0.007

de Korte et al, Circulation. 2002



In vivo validation IV

- Relation between strain and vulnerable plaque markers.

Presence of a high strain spot

	fat	no fat
↑ e	9	3
↓ e	0	12

	MΦ	no MΦ
↑ e	11	1
↓ e	1	11

de Korte et al, Circulation. 2002

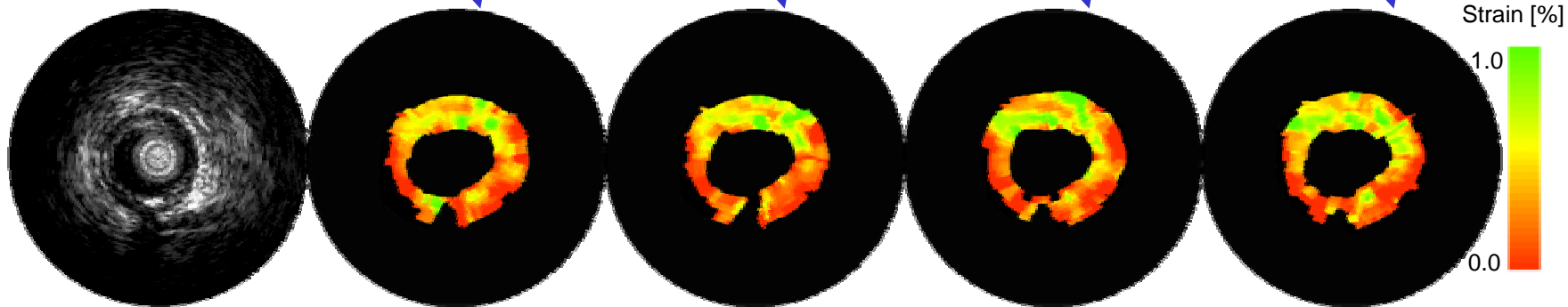
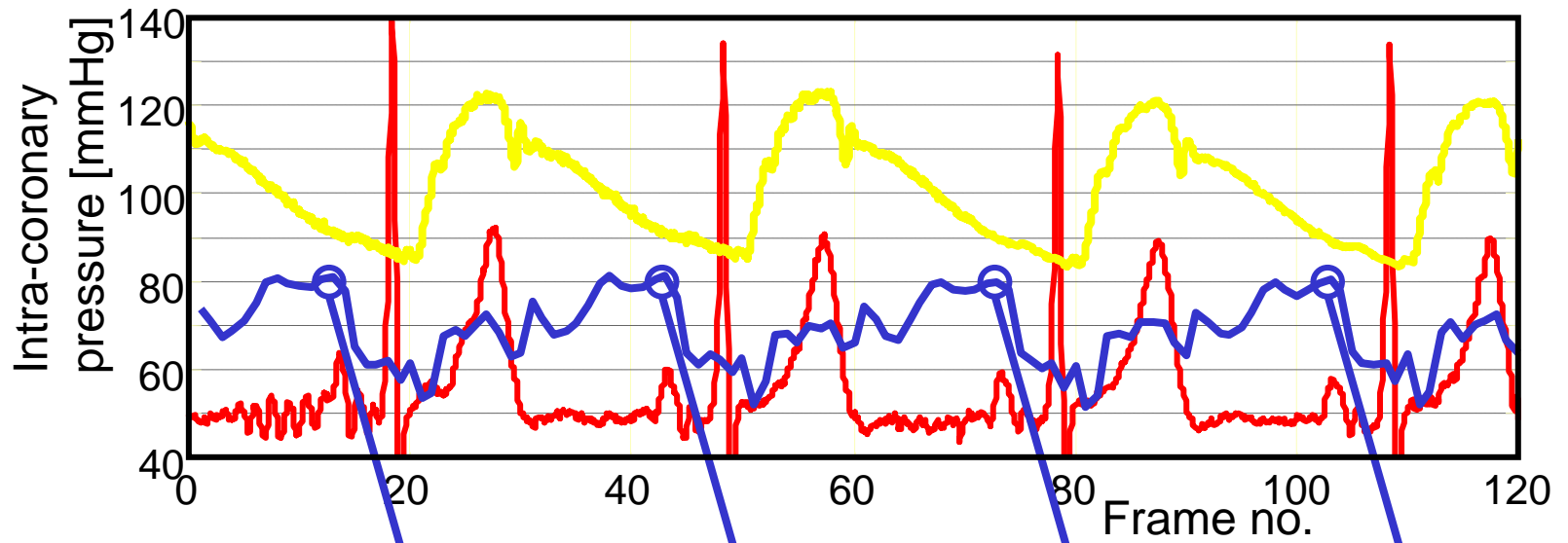


Patient studies

- Patients referred for Percutaneous Coronary intervention
- Pre intervention IVUS assessment of the culprit lesion using array catheter connected to commercial IVUS echo system.
- Due to contraction of the heart the catheter will have in-plane and out-of-plane motion:
Find phase of heart-cycle with minimal motion.



Patient studies II

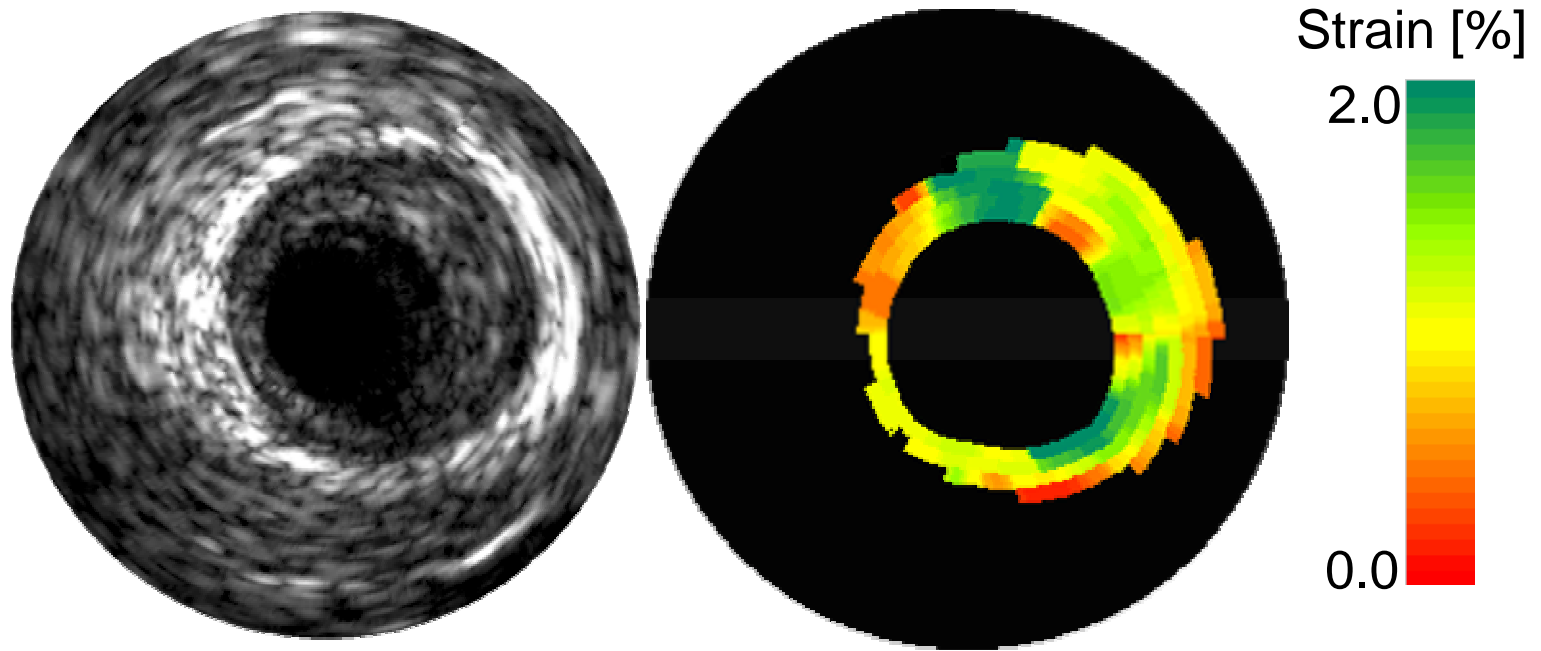


de Korte et al, Eur Heart J. 2002



Patient studies III

- Coronary artery in patient with unstable angina pectoris

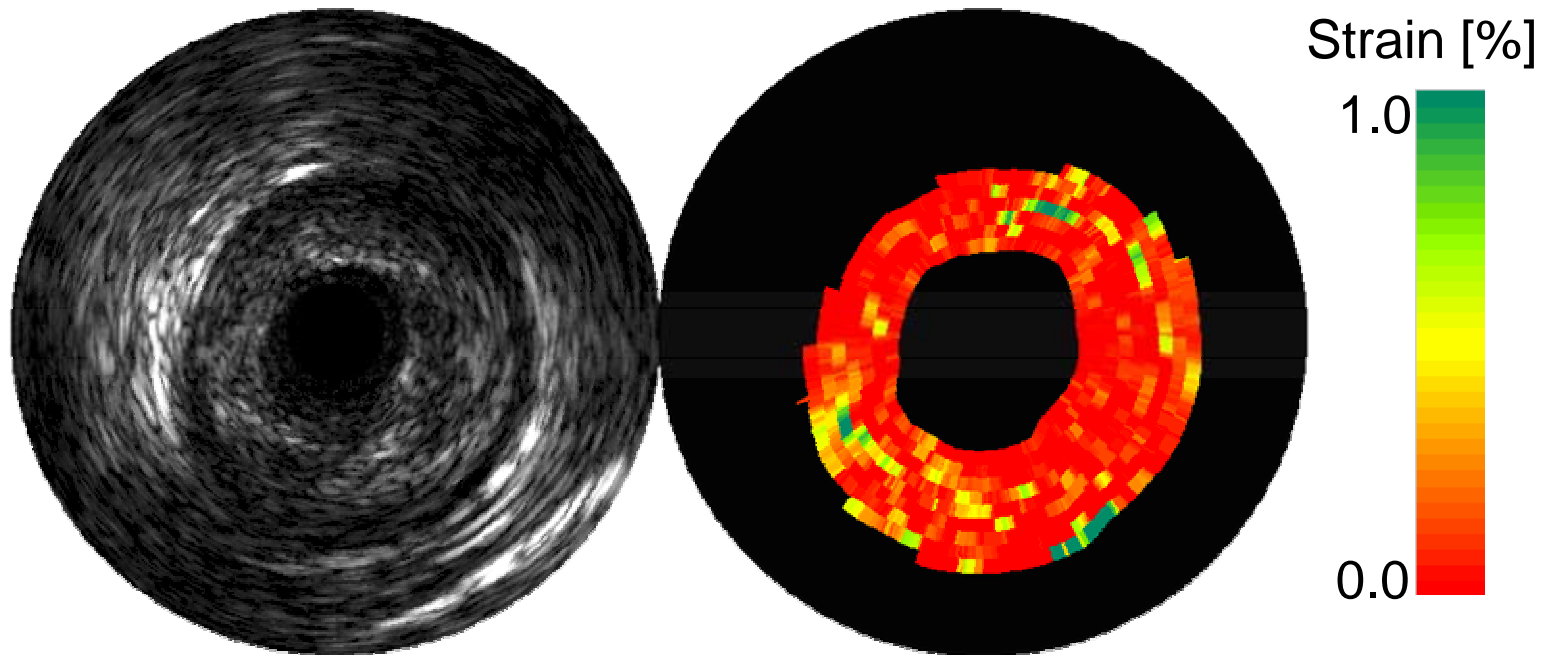


de Korte et al, WCU Proceedings. 2003



Patient studies IV

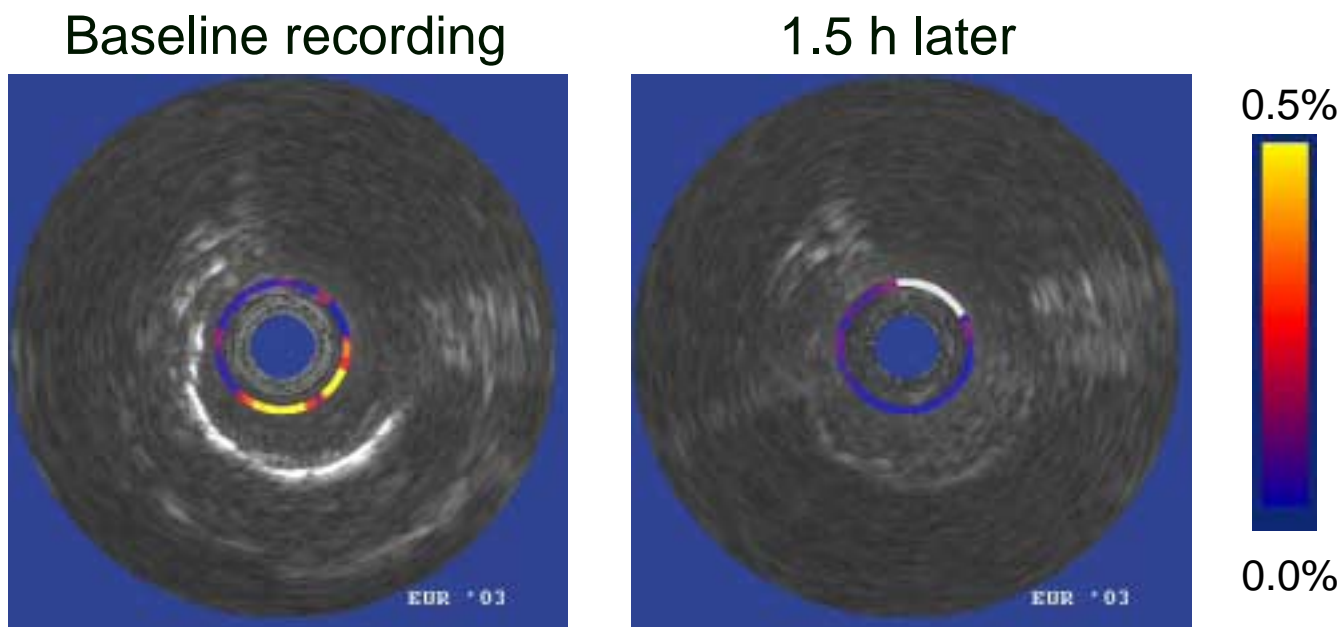
- Coronary artery in patient with stable angina pectoris





Assessment of thrombus stiffness I

- Using an intravascular array catheter as imaging device and the pulsatile pressure as force.

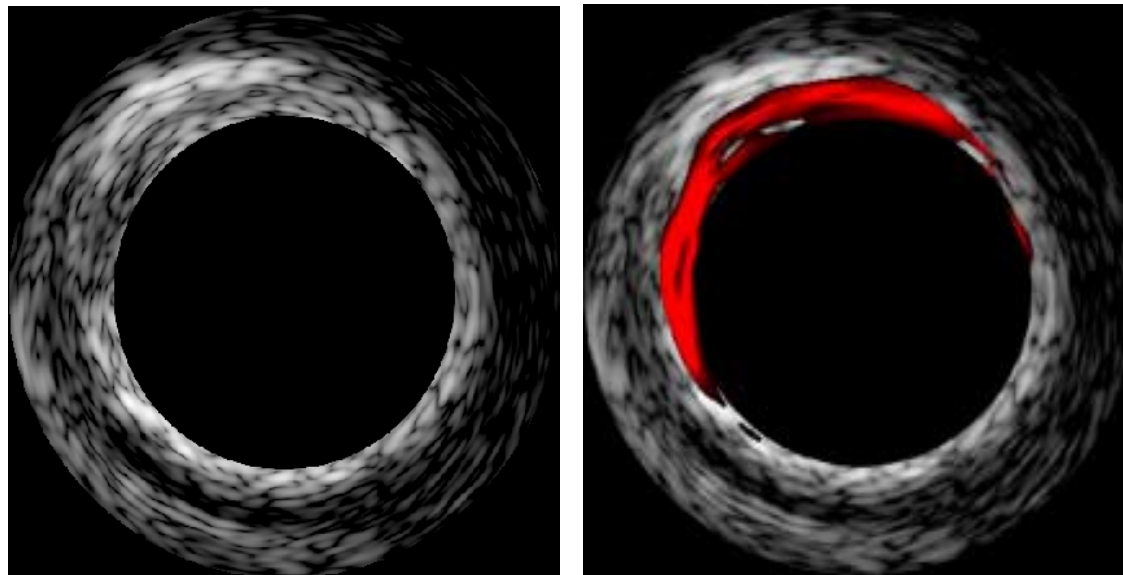


Courtesy J.A. Schaar et al, ErasmusMC, Rotterdam The Netherlands



Assessment of thrombus stiffness II

- Using an intravascular array catheter as imaging device covered by balloon as force.



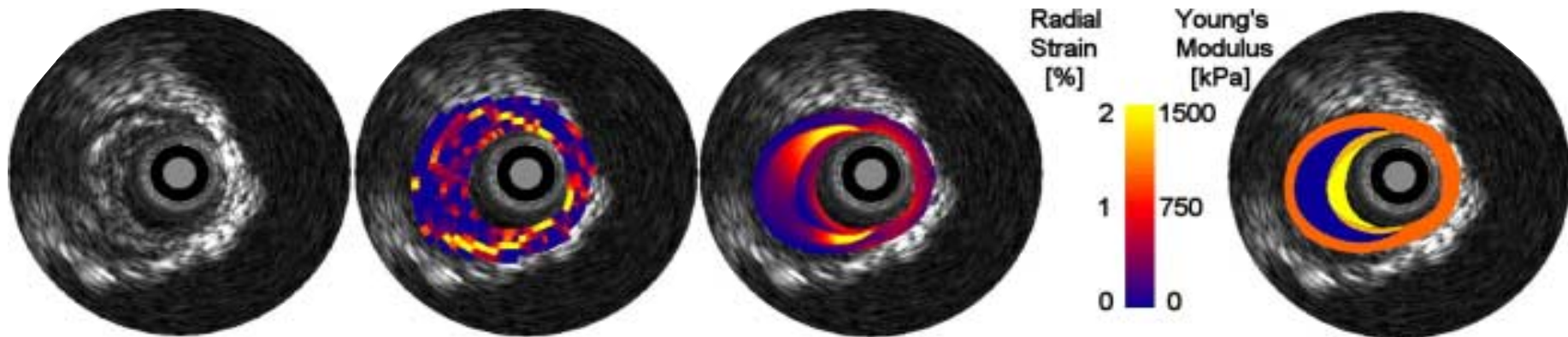
10 %  35 %

Courtesy M. O'Donnell et al, Ann Arbor, USA



Young's modulus reconstruction

- Creation of FEM using the IVUS geometry
- Parameter variation for E of cap, lipid pool and vessel wall
- Variation of cap thickness

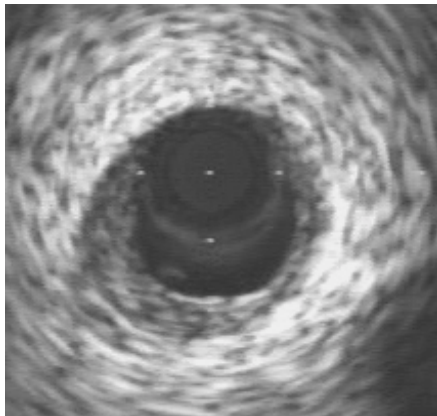


Baldewsing et al, Ultras Imag. 2004

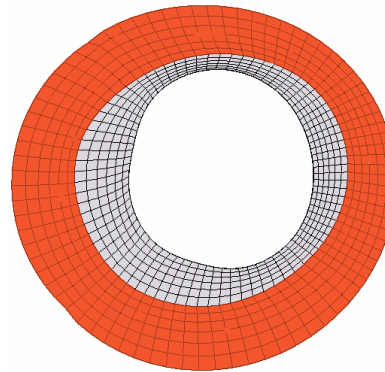


Strain calculation using Deformable Images

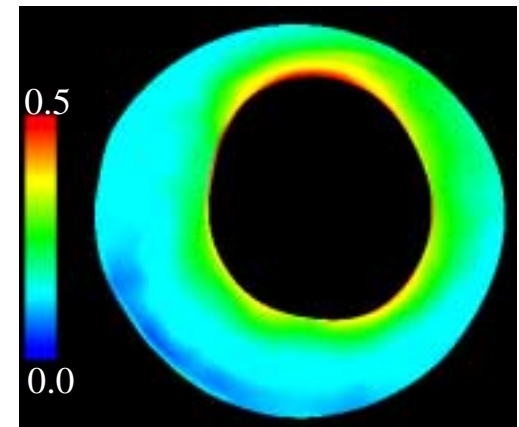
- Deformation map from Forward FE model to Template to generate synthetic Target image.
- deformation map from Forward FE model to Template to generate synthetic Target image.



Template Image



Deformed Mesh



1st principal Green-Lagrange strain

Courtesy Veress et al, Univ Utah, UT, USA

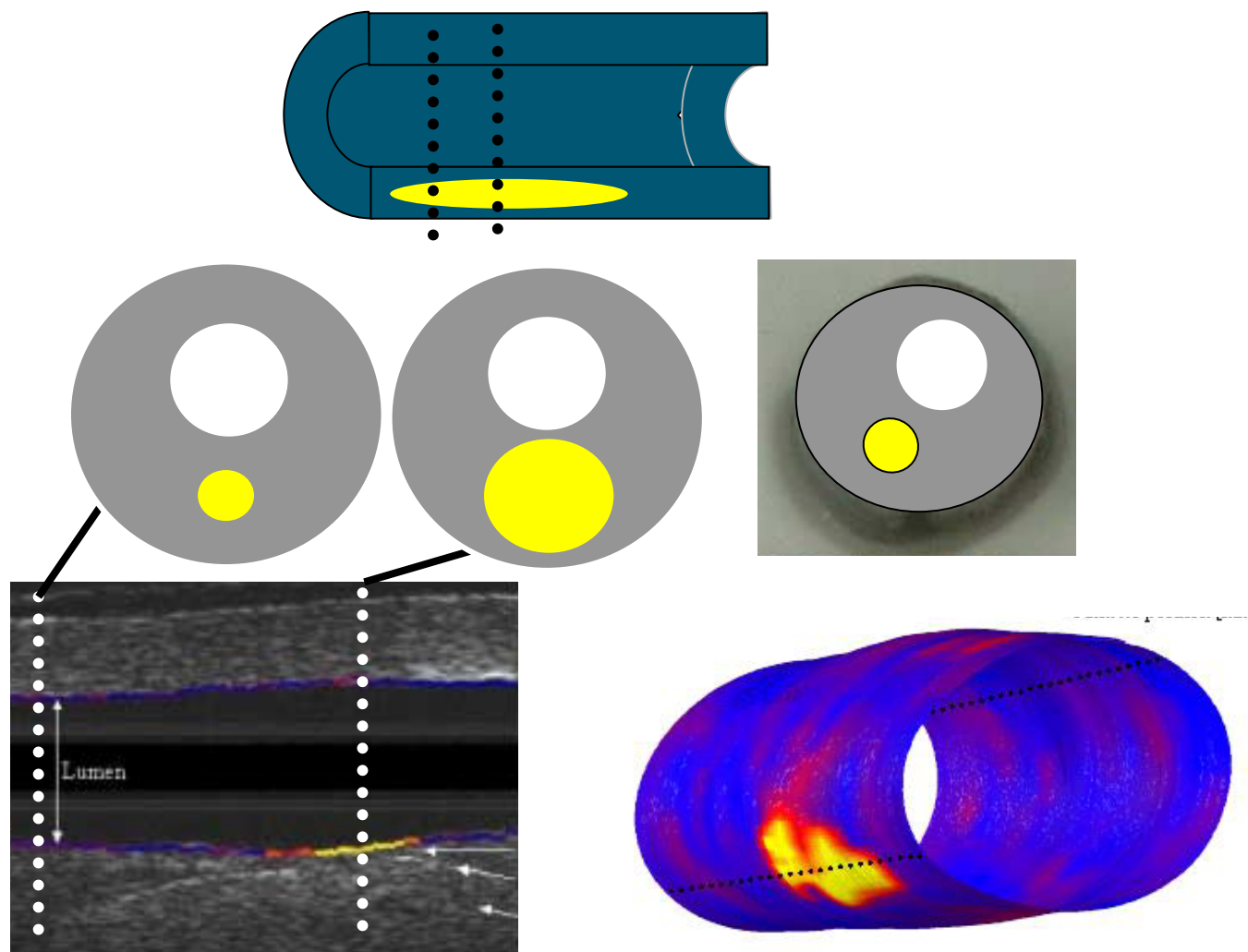


6. Three dimensional vascular elasticity imaging

- One cross-section does not represent whole artery.
- For follow-up studies, 3D information is crucial.
- Image formation of 3D artery with strain in the wall is complicated.
- Palpogram reveals strain at lumen vessel-wall boundary: most important identifier vulnerable plaque.
- In coronary artery: performing a pullback decreases out-of-plane motion.
- Each heartbeat a palpogram is calculated: depending on pullback speed a resolution of 0.5 or 1.0 mm is obtained.

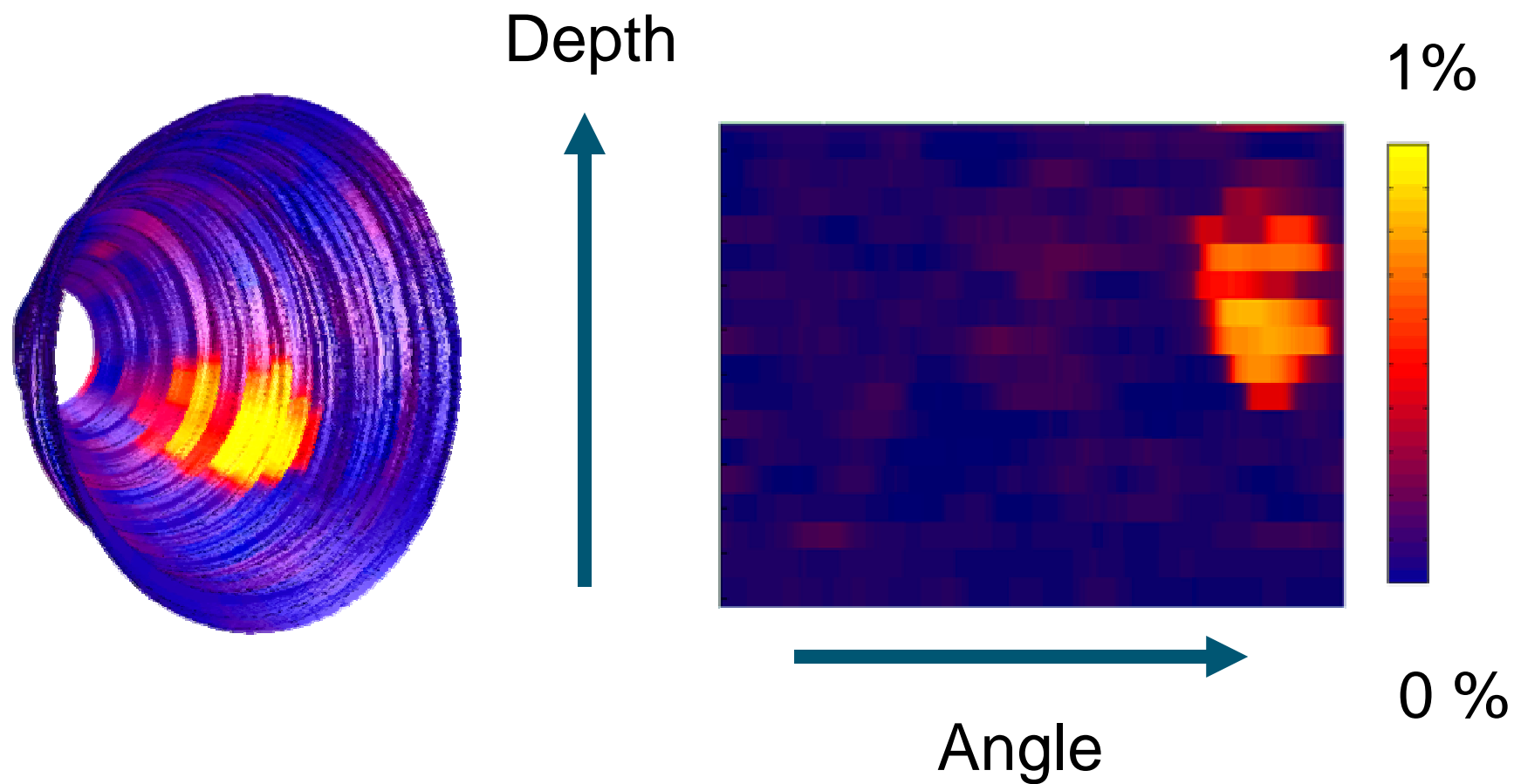


Phantom experiment I



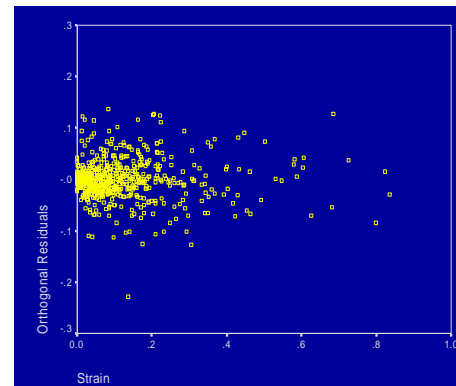
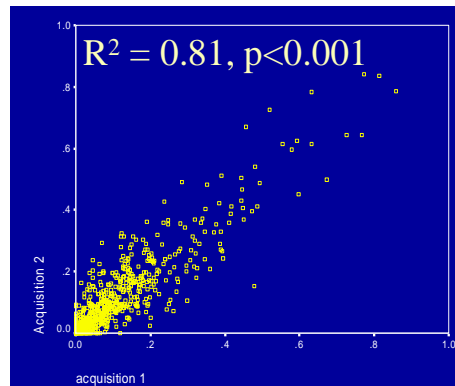
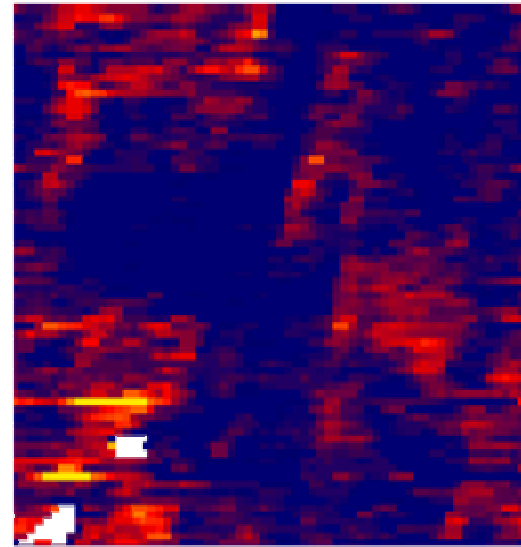
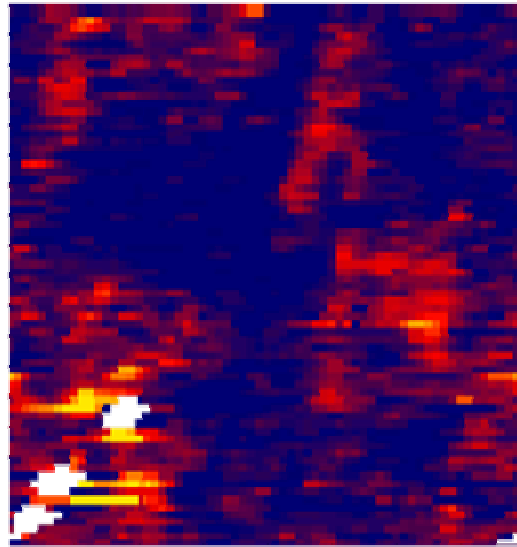


Phantom experiment II

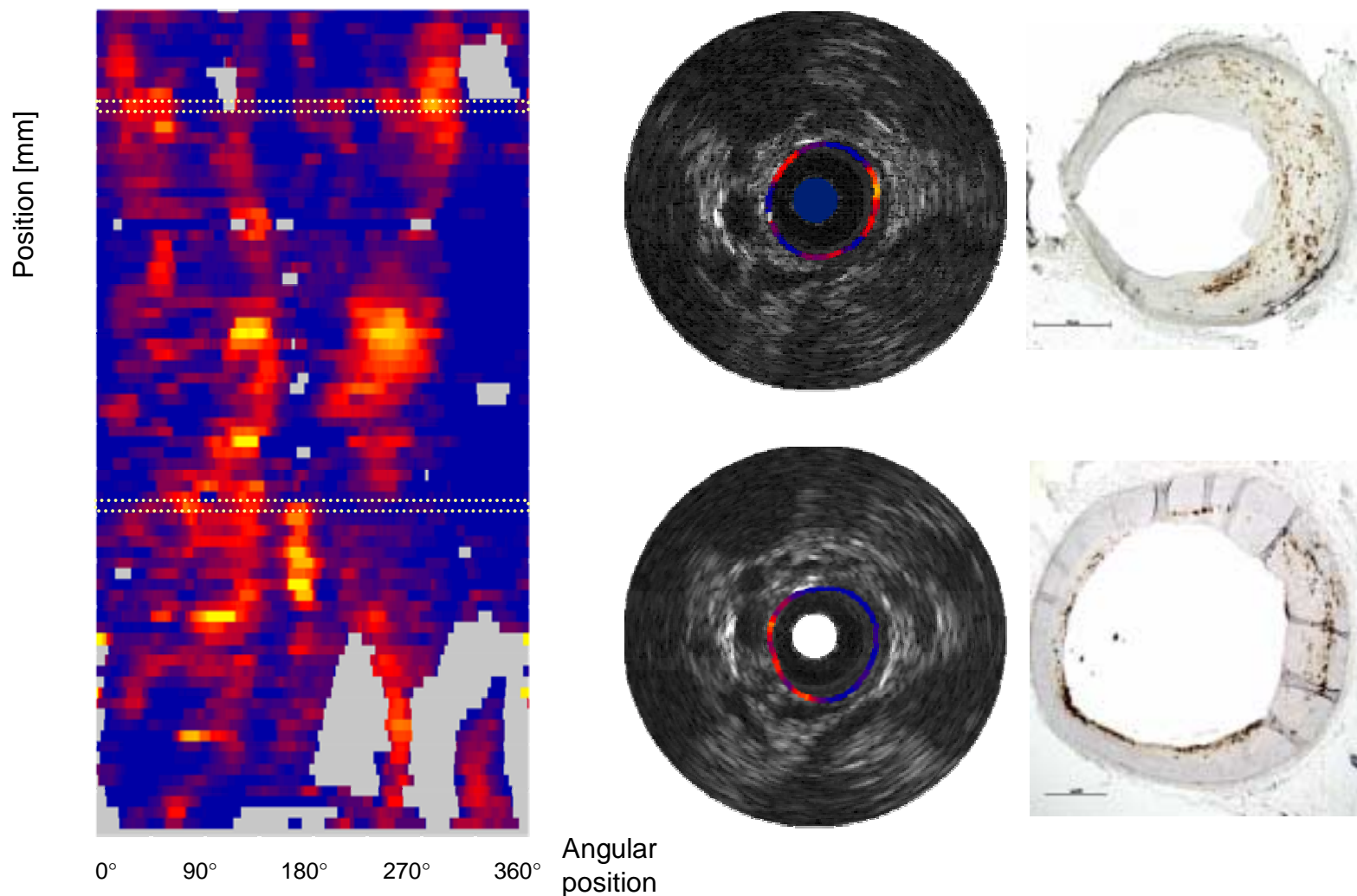




In vivo reproducibility: atherosclerotic rabbit model

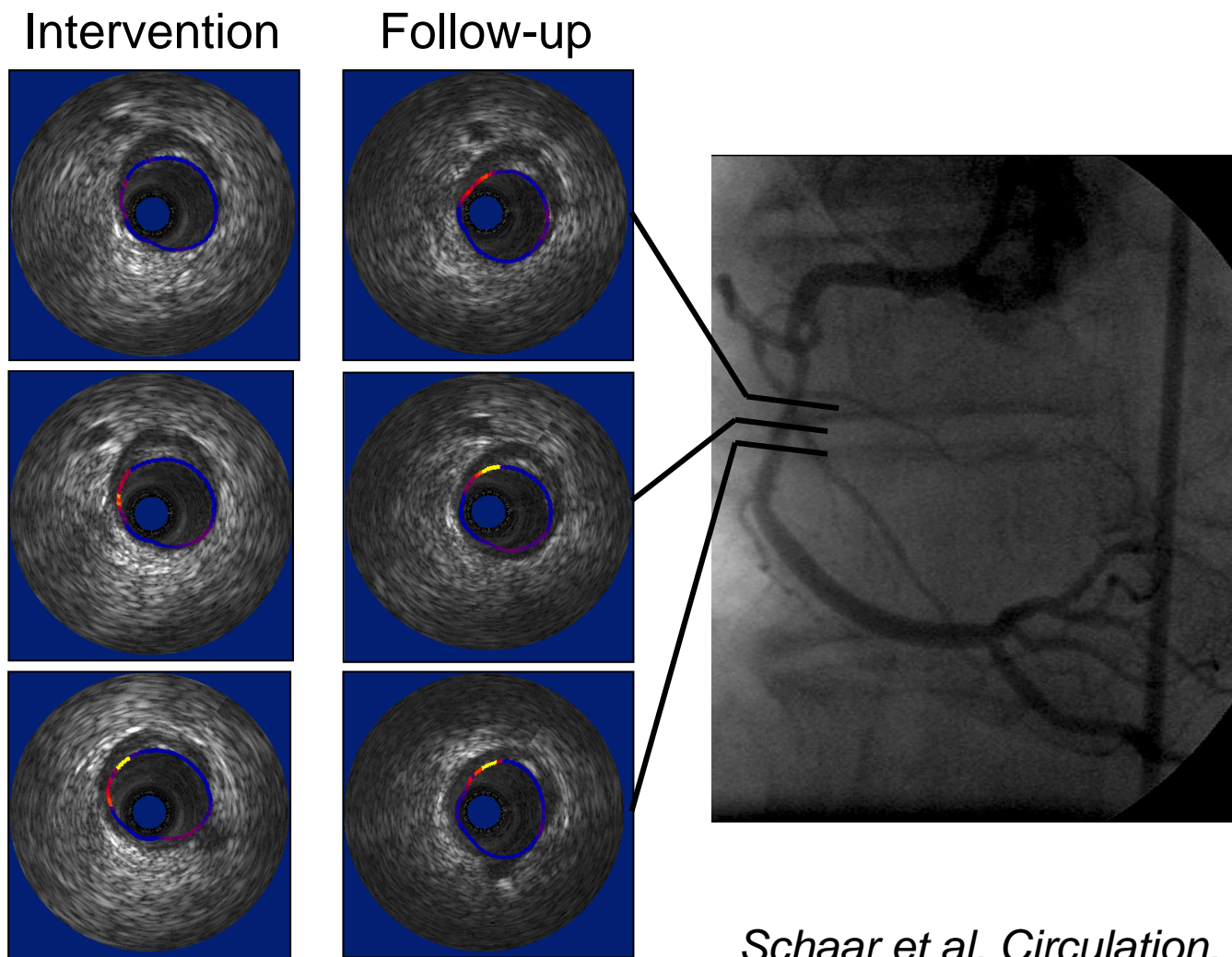


In vivo validation: atherosclerotic rabbit model





In vivo validation: follow up in patient





Conclusions

- (Intra)vascular elasticity imaging reveals information to identify thrombus age and plaque composition.
- (Intra)vascular elastography is validated in phantoms, in vitro and in vivo.
- Intravascular elastography is a powerful technique to identify the vulnerable plaque.
- Three dimensional intravascular elastography opens possibilities to perform longitudinal studies.



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